

APPLICATION FOR UNITED STATES LETTERS PATENT

of

Thomas D. Lyster

Thomas Solosko, Carlton B. Morgan, Kim J. Hansen, Daniel J.
Powers, Hans Patrick Griesser, Eric L. Jonsen, David E. Snyder

for

**MEDICAL ELECTRODE AND RELEASE LINER
CONFIGURATIONS FACILITATING PACKAGED ELECTRODE
CHARACTERIZATION**

File No. 10010201-1 (1727-35)

Certificate of Mailing Under 37 C.F.R. § 1.10

Express Mail Label No. ET450406115US Date of Deposit: 9-14-01

I hereby certify that this paper or fee is being deposited with the United States Postal Service "Express Mail Post Office to Addressee" service under 37 C.F.R. § 1.10 on the date indicated above and is addressed to: Commissioner for Patents, BOX PATENT APPLICATION, Washington, DC 20231.

Stephanie Caf

MEDICAL ELECTRODE AND RELEASE LINER CONFIGURATIONS FACILITATING PACKAGED ELECTRODE CHARACTERIZATION

BACKGROUND OF THE INVENTION

FIELD OF THE INVENTION

- 5 **[1]** The present invention relates generally to the testing of medical electrodes that are mounted on a release liner. More particularly, the invention is directed to various electrode and/or release liner embodiments that facilitate testing and characterization of packaged electrodes.

DESCRIPTION OF THE BACKGROUND ART

- 10 **[2]** Sudden Cardiac Arrest (SCA) is one of the leading causes of death in the industrialized world. SCA typically results from an arrhythmia condition known as Ventricular Fibrillation (VF), during which a patient's heart muscle exhibits extremely rapid, uncoordinated contractions that render the heart incapable of circulating blood. Statistically, after four minutes have elapsed, the patient's chance of survival
15 decreases by 10% during each subsequent minute they fail to receive treatment.

- 20 **[3]** An effective treatment for VF is electrical defibrillation, in which a defibrillator delivers an electrical pulse, waveform, or shock to the patient's heart. Because the onset of VF is generally an unpredictable event, the likelihood that a victim will survive increases dramatically if 1) defibrillation equipment is nearby; 2) such equipment is in proper working order; and 3) such equipment may be easily, rapidly, and effectively deployed to treat the patient.

- 25 **[4]** Medical equipment manufacturers have developed Automated External Defibrillators (AEDs) that minimally trained personnel may use to perform electrical defibrillation when emergency situations arise. AEDs may be found in a variety of non-medical settings, including residences, public buildings, businesses, private vehicles, public transportation vehicles, and airplanes.

- [5]** An AED relies upon a set of electrodes to deliver a series of shocks to a patient. An electrode therefore serves as a physical and electrical interface between the AED and the patient's body. In general, an electrode may comprise a conductive

foil layer that resides upon a conductive adhesive layer; a lead wire that couples the foil layer to the AED; and an insulating layer that covers the foil layer. The conductive adhesive layer physically and electrically interfaces the foil layer to a patient's skin. New or unused electrodes reside upon a release liner, from which an operator may peel off an electrode prior to placement upon a patient's body. During manufacture, electrodes upon their release liner are typically sealed in a package.

[6] An AED is likely to be used infrequently; however, any given use may involve a time critical, life threatening situation. Thus, it is imperative that the AED be able to provide an indication of its operating condition at essentially any time. While in a quiescent state, an AED generally performs periodic diagnostic sequences to determine its current operating condition. Such sequences may be performed, for example, on a daily and/or weekly basis. The diagnostic sequences include tests for characterizing the current path between the AED and a set of electrodes. Hence, the electrodes must be connected to the AED while the AED is in its quiescent state, and the electrodes must be electrically testable while mounted on their release liner. As a result, release liners providing electrical contact between electrodes have been developed.

[7] Such release liners generally include multiple openings that facilitate electrical contact between electrodes. The current path between the AED and the electrodes includes each electrode's lead wire, foil layer, and conductive adhesive layer. For a pair of new, properly functioning conventional electrodes mounted upon a release liner having multiple openings, this current path may be characterized by an impedance value ranging between 2 and 10 Ohms. If an impedance measurement indicates an electrical discontinuity or open circuit condition exists, a lead wire or connector coupling an electrode to the AED may be damaged, and/or an electrode may be improperly connected to the AED. Similarly, if an impedance measurement indicates a short or open circuit condition exists, one or more electrodes, a lead wire or other wire within the current path, and/or a connector that couples the electrodes to the AED may be damaged or defective.

[8] A measurement indicating a higher than desired impedance may arise when an electrode is damaged, deteriorated, and/or degraded. An electrode's

conductive adhesive layer typically comprises a hydrogel film, which itself comprises natural and/or synthetic polymers dispersed or distributed in an aqueous fluid. The electrical properties of the hydrogel film are dependent upon its moisture content. If the hydrogel possesses appropriate water content, it provides a low impedance electrical path between the electrode's foil layer and a patient's skin. The hydrogel film, however, dries out over time. As a result, its impedance increases over time, thereby undesirably decreasing its effectiveness for signal exchange and energy transfer between a patient and an AED. Once moisture loss has reached a certain level, the hydrogel film, and hence the electrode of which it forms a part, may be unsuitable for use.

[9] A patient's transthoracic impedance typically falls within a range of 25 to 200 Ohms. As electrodes' hydrogel film deteriorate over time, the impedance associated with the electrical path provided by the electrodes may overlap with the typical transthoracic impedance range. Thus, if an AED in a normal operational or "on" state measures an electrode impedance corresponding to a patient's transthoracic impedance, the AED has no inherent way of determining whether partially deteriorated electrodes are currently mounted upon their release liner, or properly functioning electrodes are connected to the patient.

[10] Prior release liners that facilitate electrical testing of electrodes mounted thereupon have typically been unnecessarily complex, expensive to manufacture, unacceptable relative to difficulty of electrode removal, and/or limited relative to the extent to which they permit accurate characterization of an electrode's hydrogel film. A need exists for electrodes and/or release liners that overcome the aforementioned deficiencies.

SUMMARY OF THE INVENTION

[11] The present invention includes a number of release liner, electrode, and/or medical or measuring device embodiments that facilitate electrical characterization of one or more electrodes coupled to the medical or measuring device. In the context of the present invention, a medical device may be essentially any device capable of using electrodes to receive signals from and/or deliver signals

and/or energy to a patient's body. A measuring device may be essentially any device capable of electrically characterizing packaged electrodes.

[12] In one embodiment, a release liner comprises a release layer and a moisture-permeable and/or moisture-absorbent membrane or sheet. The release layer may include an opening therein, over which the membrane may reside. When electrodes are positioned or mounted upon the release liner, the electrodes' conductive adhesive or hydrogel layers may transfer moisture to the membrane, thereby forming a low impedance electrical path that facilitates electrical communication between electrodes. The membrane may be prewetted or premoistened prior to mounting electrodes upon the release layer to minimize electrode moisture loss.

[13] The release layer may comprise a single, foldable sheet that surrounds or partially surrounds the membrane. A pair of electrodes residing upon the same side of the foldable sheet may exchange electrical signals. Alternatively, a first and a second release layer may encase or enclose one or more portions of the membrane, where each release layer includes an opening. In another release liner embodiment, a membrane may extend beyond a border of a single release layer that lacks openings. Electrodes mounted upon the release layer in such an embodiment also extend beyond the release layer border, and contact the membrane to facilitate electrical communication therebetween.

[14] A release liner and electrode package according to an embodiment of the invention may comprise a rigid cartridge having an electrical interface incorporated therein; a release liner having a set of openings therein; and a set of electrodes mounted upon the release liner. The openings in the release liner facilitate electrical communication between electrodes. The rigid cartridge provides an environment characterized by well-defined internal conditions, where moisture transfer in or out of the rigid cartridge is minimal or essentially eliminated. Such a package may therefore prolong electrode lifetime.

[15] A release liner according to another embodiment of the invention may comprise a release layer upon which a conductive strip resides. Electrodes may be mounted in a side-by-side manner upon the release layer, and may exchange

electrical signals via the conductive strip. The release layer may comprise a foldable sheet. In an alternate embodiment, the conductive strip may wrap around or encircle the release layer, facilitating electrical communication between electrodes mounted on opposite sides of the release layer.

- 5 **[16]** A release liner according to another embodiment of the invention may comprise a release layer having a set of openings therein, and a conductive backing layer. The release layer may comprise a foldable sheet. Electrodes may be mounted upon such a release liner in a side by side manner. An electrical signal may travel from one electrode, through an opening in the release layer, through or within
10 the conductive backing layer, through another opening in the release layer, and into another electrode.

[17] The conductive backing layer may comprise a metal, or a conductive adhesive layer such as a hydrogel layer. In the event that the conductive backing layer comprises a conductive adhesive layer, an electrical current traveling between
15 mounted electrodes may follow a path that is much greater than the thickness of the electrodes' conductive adhesive layers. As a result, the measured impedance of the release liner may be greater than typical patient impedance ranges, and may exhibit a high degree of sensitivity to conductive adhesive layer degradation over time.

- [18]** A release liner according to another embodiment of the invention may comprise a first release layer or sheet, a second release layer or sheet, and an intervening conductive adhesive layer. The first and second release layers each include an opening. The first and second release layers are oriented or positioned such that their openings are offset relative to each other by a separation distance. Electrodes mounted upon the release layers may exchange electrical signals with
25 each other via the release layer openings and the conductive adhesive layer between the release layers. Such electrical signals may travel through a length of conductive adhesive layer that is much greater than the thickness of the electrodes' conductive adhesive layers, in a manner analogous to that described above. In an alternate embodiment, a release liner may comprise a foldable sheet that surrounds or
30 encases one or more portions of a conductive adhesive or hydrogel layer. The foldable sheet may include openings, which are offset relative to each other in

accordance with a given separation distance when the foldable sheet surrounds or encases portions of the conductive adhesive layer.

[19] An electrode according to an embodiment of the invention may comprise a conductive adhesive layer coupled to a conductive foil layer that includes one or more voids therein. Each void affects electrical current flow through the electrode's conductive adhesive layer when the electrode is mounted upon a release liner that facilitates electrical communication between electrodes. In particular, the presence of a void may cause transverse electrical current flow through the electrode's conductive adhesive layer, rather than simply current flow through the conductive adhesive layer's thickness. This results in a longer electrical path, which in turn may provide the voided electrode with an impedance that is greater than typical patient impedance levels. Additionally, impedance measurements along this electrical path may exhibit a significant degree of sensitivity to changes in conductive adhesive layer properties over time.

[20] An electrode may include or incorporate one or more insulating switches between its conductive foil layer and conductive adhesive layers. When the electrode is mounted upon a release liner that facilitates electrical communication between electrodes, the presence of an insulating switch may result in transverse current flow through the electrode's conductive adhesive layer in a manner analogous to that described above for the voided electrode.

[21] An electrode according to another embodiment of the invention may comprise a conductive foil layer, a conductive adhesive layer, and a sonomicrometer or ultrasonic transducer. When electrodes that incorporate ultrasonic transducers are mounted upon a release liner, ultrasonic signals transmitted and/or received via the ultrasonic transducers may be used to indicate an electrode separation distance. The electrode separation distance may indicate whether electrodes are mounted upon a release liner or a patient's body.

[22] In accordance with the present invention, various types of electrodes may be mounted upon release liners that facilitate exchange of electrical signals between electrodes. A medical device to which such electrodes are coupled may perform a variety of measurements to characterize electrode condition or fitness for

use. The medical device may measure a short or open circuit condition, which may indicate an electrical path problem. As one or more electrodes' conductive adhesive layers degrade over time, the medical device may measure increasing impedance levels. If an impedance level exceeds a given threshold value or range, the medical device may provide an indication that the electrodes are non-optimal or unfit for use. The medical device may alternately or additionally provide an indication of electrode condition or fitness for use at particular times or time intervals. The medical device may further calculate or determine a time remaining before an electrode or electrode pair may no longer be fit for use. Such a calculation or determination may be based upon a current degradation curve.

[23] In accordance with an embodiment of the invention, a release liner that lacks openings may serve as a capacitive medium between electrodes mounted thereupon. A medical device may perform a capacitance measurement to electrically characterize an electrical path corresponding to the electrodes and release liner.

[24] In accordance with another embodiment of the invention, a release liner may comprise a release layer that includes an opening, and an insulating switch or patch that covers or resides within the opening. Electrodes may be mounted upon the release layer such that the electrodes' conductive adhesive layers cover the opening, and at least one electrode's conductive adhesive layer covers the switch.

[25] A medical device may perform a complex impedance measurement upon electrodes mounted upon a release liner having such a switch. When one or more such electrodes include a void or internal switch as described above, the result of the complex impedance measurement may exhibit significant dependence upon the current condition of such electrodes' conductive adhesive layers. The medical device may therefore determine an extent to which one or more electrodes are fit for use. The medical device may further provide a visual and/or other indication of electrode condition and/or fitness for use.

[26] A medical device such as an Automated External Defibrillator (AED) may include or incorporate elements for periodically determining electrode condition or status. The medical device may include a status measurement unit, which may operate in conjunction with an electrode condition indicator, a display device, a

speaker, and/or other elements in a variety of manners to indicate electrode condition, fitness for use, and/or an estimated remaining electrode lifetime. In accordance with an embodiment of the invention, an electrode condition indicator may incorporate, generate, and/or present one or more types of visual metaphors that provide an indication of electrode status, condition, and/or estimated remaining lifetime. A visual metaphor may correspond to a fuel gauge, and may convey positional and/or color relationships between one or more indicating elements that change or vary over time in accordance with measured and/or estimated electrode properties. The visual metaphor may further convey textual and/or symbolic information.

BRIEF DESCRIPTION OF THE DRAWINGS

- [27] FIG. 1A is a layered perspective view of a release liner according to an embodiment of the invention.
- [28] FIG. 1B is a perspective view of electrodes mounted upon the release liner of FIG. 1A.
- [29] FIG. 1C is a perspective view of a release liner according to another embodiment of the invention, and a manner of mounting electrodes thereupon.
- [30] FIG. 2A is a perspective view of a release liner according to another embodiment of the invention.
- [31] FIG. 2B is a perspective view of electrodes mounted upon the release liner of FIG. 2A.
- [32] FIG. 3A is a layered perspective view of a release liner according to another embodiment of the invention.
- [33] FIG. 3B is a perspective view of electrodes mounted upon the release liner of FIG. 3A.
- [34] FIG. 4 is a perspective view of a release liner and an electrode package according to an embodiment of the invention.
- [35] FIG. 5A is a plan view of a release liner according to another embodiment of the invention.

[36] FIG. 5B is a plan view of electrodes mounted upon the release liner of FIG. 5A.

[37] FIG. 6A is a perspective view of another embodiment of a release liner according to the invention.

5 [38] FIG. 6B is a perspective view of electrodes mounted upon the release liner of FIG. 6A.

[39] FIG. 7 is a perspective view of a release liner according to another embodiment of the invention, and a manner of mounting electrodes upon the same.

10 [40] FIG. 8A is a layered perspective view of a release liner according to another embodiment of the invention.

[41] FIG. 8B is a perspective view of electrodes mounted upon the release liner of FIG. 8A.

[42] FIG. 9A is a perspective view of a release liner according to another embodiment of the invention.

15 [43] FIG. 9B is a perspective view showing electrodes mounted upon the release liner of FIG. 9A.

[44] FIG. 10A is a layered plan view of a release liner according to another embodiment of the invention.

20 [45] FIG. 10B is a perspective view of electrodes mounted upon the release liner of FIG. 10A.

[46] FIG. 11A is a perspective view of a release liner according to another embodiment of the invention.

[47] FIG. 11B is a perspective view of electrodes mounted upon the release liner of FIG. 11A.

25 [48] FIG. 12A is a cross sectional view of an electrode according to an embodiment of the invention.

[49] FIG. 12B is a plan view of the electrode of FIG. 12A.

[50] FIG. 12C is a plan view of an electrode according to another embodiment of the invention.

[51] FIG. 12D is a cross sectional view of an electrode according to another embodiment of the invention.

5 [52] FIG. 12E is a plan view of the electrode of FIG. 12D.

[53] FIG. 13A is a graph of exemplary current density relative to lateral position for a conventional electrode mounted upon a patient's body.

[54] FIG. 13B is a graph of exemplary current density relative to lateral position beneath elements of the electrode of FIG. 12A when the electrode is
10 mounted upon a patient's body.

[55] FIG. 14A is a perspective view of electrodes of FIG. 12A mounted upon a release liner according to another embodiment of the invention.

[56] FIG. 14B is a cross sectional view of electrodes of FIG. 12A mounted upon the release liner of FIG. 14A.

15 [57] FIG. 15 is a plan view of the electrode of FIG. 12A and a conventional electrode mounted upon the release liner of FIG. 8A.

[58] FIG. 16 is a plan view of electrodes of FIG. 12D mounted upon the release liner of FIG. 8A.

[59] FIG. 17 is a cross sectional view of an electrode according to another
20 embodiment of the invention.

[60] FIG. 18 is a perspective view of electrodes of FIG. 17 mounted upon the release liner of FIG. 14A.

[61] FIG. 19 is a perspective view of electrodes of FIG. 12C and a conventional electrode mounted upon a release liner according to another
25 embodiment of the invention.

[62] FIG. 20 is a perspective view of electrodes mounted upon a release liner in accordance with another embodiment of the invention.

[63] FIG. 21A is a plan view of a release liner according to another embodiment of the invention.

[64] FIG. 21B is a perspective view of electrodes mounted upon the release liner of FIG. 21A.

5 [65] FIG. 21C is a cross sectional view of an electrode to release liner assembly of FIG. 21B.

[66] FIG. 21D is an equivalent circuit corresponding to the electrode to release liner assembly of FIG. 21B.

10 [67] FIG. 22A is a perspective view of an electrode of FIG. 12A and a conventional electrode mounted upon the release liner of FIG. 21A.

[68] FIG. 22B is a cross sectional view of a voided electrode to release liner to conventional electrode assembly of FIG. 22A.

[69] FIG. 22C is an equivalent circuit corresponding to the voided electrode to release liner to conventional electrode assembly of FIG. 22A.

15 [70] FIG. 23A is a perspective view of electrodes of FIG. 12A mounted upon the release liner of FIG. 21A.

[71] FIG. 23B is a cross sectional view of a voided electrode to release liner to voided electrode assembly of FIG. 23A.

20 [72] FIG. 23C is an equivalent circuit corresponding to the voided electrode to release liner to voided electrode assembly of FIG. 23A.

[73] FIG. 24A is a layered plan view of a release liner according to another embodiment of the invention.

[74] FIG. 24B is a plan view of a conventional electrode and an electrode of FIG. 12A mounted upon the release liner of FIG. 24A.

25 [75] FIG. 25A is a plan view of a release liner according to another embodiment of the invention.

[76] FIG. 25B is a perspective view of electrodes of FIG. 12A mounted upon the release liner of FIG. 25A.

[77] FIG. 26 is a perspective view of a release liner according to another embodiment of the invention, and electrodes of FIG. 12A mounted thereupon.

[78] FIG. 27 is a block diagram of an Automated External Defibrillator coupled to a set of electrodes mounted upon a release liner in accordance with the present invention.

[79] FIG. 28A is an illustration of an electrode condition indicator in accordance with an embodiment of the invention.

[80] FIG. 28B is an illustration of an electrode condition indicator in accordance with another embodiment of the invention.

[81] FIG. 29A is an illustration of a remaining time indicator in accordance with an embodiment of the invention.

[82] FIG. 29B is an illustration of a remaining time indicator in accordance with another embodiment of the invention.

[83] FIG. 30 is a perspective view of a package incorporating an electrode condition and/or remaining time indicator and electrodes mounted upon a release liner.

[84] FIG. 31 is a block diagram of an Automated External Defibrillator that includes an electrode condition indicator and/or an estimated remaining electrode lifetime indicator.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[85] The following discussion is presented to enable a person skilled in the art to make and use the invention. The general principles described herein may be applied to embodiments and applications other than those detailed below without departing from the spirit and scope of the present invention as defined by the appended claims. The present invention is not intended to be limited to the embodiments shown, but is to be accorded the widest scope consistent with the principles and features disclosed herein.

[86] The present invention encompasses a wide variety of release liner and/or electrode embodiments that facilitate automatic electrical characterization of

one or more packaged electrodes coupled to a medical or measuring device. In the context of the present invention, a medical device may be essentially any type of device capable of employing a set of electrodes to exchange signals with a patient. For example, the medical device may be a defibrillator; a cardiac pacing system; an electrocardiograph (ECG) or patient monitoring system; or an electrosurgery device. Since electrode fitness is of particular concern in relation to medical devices designed to provide emergency resuscitation capabilities, the description herein most commonly considers release liners and/or electrodes suitable for deployment with defibrillators, particularly Automated External Defibrillators (AEDs).

[87] Relative to the present invention, a measuring device may be essentially any type of device capable of performing electrical measurements upon electrodes designed and/or packaged or mounted upon a release liner in accordance with the present invention. A measuring device need not include patient monitoring and/or treatment elements, but may comprise, for example, a power supply and a multi-meter. Alternatively, a measuring device may comprise an LCR meter. Portions of the description herein that refer to packaged electrode characterization via a medical device may apply equally to packaged electrode characterization via a measuring device.

[88] With respect to any or essentially any of the electrode and/or release liner embodiments described herein, a medical or measuring device may perform electrical characterization measurements and/or tests via conductive pathways, lead wires, and/or connectors associated with normal electrode configurations and/or normal electrode use. That is, the electrode and/or release liner embodiments detailed herein may require no additional couplings to a medical or measuring device beyond those that facilitate normal signal exchange between a patient and a medical device.

[89] In accordance with the present invention, a medical or measuring device may include temperature measurement and/or compensation circuitry or elements to account and/or compensate for the effects of temperature variations upon the measured values of electrical parameters. A medical or measuring device may adjust electrical measurement and/or test parameters or criteria based upon one

09954750-091401

or more temperature measurements to facilitate temperature compensated characterization of electrodes mounted upon a release liner. Temperature compensation capabilities may be of particular value in medical or measuring devices that perform impedance measurements such as those described in detail below.

5 **[90]** A medical device operating in accordance with the present invention may also include impedance compensation circuitry, such as that described in U.S. Patent No. 6,047,212, entitled "External Defibrillator Capable of Delivering Patient Impedance Compensated Biphasic Waveforms," which is incorporated herein by reference.

10 **[91]** As described in detail below, a medical or measuring device may perform one or more types of measurements upon electrodes mounted upon a release liner. The medical or measuring device may perform in-situ measurements at various intervals over time, and provide an indication of current electrode condition and/or estimated remaining lifetime based upon such measurements. As a result, in
15 contrast to the prior art, packaged electrodes designed and/or deployed in accordance with the present invention may not require associated markings or other information to define or specify an expiration date or shelf life.

[92] Packaged electrodes designed and/or deployed in accordance with the present invention may include a wrapper, covering, label or the like that includes an
20 "install by" date that specifies a date by which electrodes should be installed upon or coupled to a medical or measuring device. The wrapper may be removed to facilitate installation, after which the medical or measuring device may determine when electrode replacement is required based upon electrical measurements.

[93] **FIG. 1A** is a layered perspective view of a release liner **100** according
25 to an embodiment of the invention. In one embodiment, the release liner **100** comprises a first release layer or sheet **110**; a second release layer or sheet **120**; and a moisture-permeable membrane **130**. The first release layer **110** includes one or more openings **112** disposed therein. Similarly, the second release layer **120** includes one or more openings **122**, which may positionally correspond to those in
30 the first release layer **110**.

[94] Each release layer **110, 120** may comprise a nonconductive sheet having non-stick properties. A given release layer **110, 120** may comprise silicon-coated paper, polyester, polypropylene, polyethylene, and/or other non-stick materials, in a manner well understood by those skilled in the art. The openings **112, 122** in each release layer **110, 120** may be cut, stamped, or punched out using conventional techniques.

[95] The moisture-permeable membrane **130** may comprise a nonconductive, moisture-permeable and/or moisture-absorbent material, such as litmus paper, that resides between the first and second release layers **110, 120**.

While the moisture-permeable membrane **130** is depicted in **FIG. 1A** as spanning an area approximately equal to that of the first and second release layers **110, 120**, the moisture-permeable membrane **130** may be smaller, subject to the requirement that it cover openings **112, 122** in the first and second release layers **110, 120**. Depending upon embodiment and/or implementation details, the moisture-permeable membrane **130** may be adhered, bonded, laminated, and/or otherwise attached to one, both, or neither release layer **110, 120**, as further detailed hereafter.

[96] In one embodiment, the release liner **100** may be manufactured such that the moisture-permeable membrane **130** is bonded, adhered, laminated, and/or otherwise attached to an inside surface of first release layer **110**. The second release layer **120** may be oriented or positioned such that its openings **122** are essentially coincident with the set of openings **112** in the first release layer **110**. Following any required positioning, the second release layer **120** may be bonded, adhered, laminated, and/or otherwise attached to the moisture-permeable membrane **130** in a manner similar to that for the first release layer **110**.

[97] **FIG. 1B** is a perspective view of electrodes **150** mounted upon the release liner **100** of **FIG. 1A**. In one embodiment, each electrode **150** may be conventional, and comprises a conductive foil layer that resides upon a conductive adhesive layer. The conductive adhesive layer may comprise a conductive gel layer, such as a hydrogel layer, in a manner well understood by those skilled in the art. In general, the electrical properties of the conductive adhesive layer may degrade over time, which may occur as a result of moisture loss, solvent loss, cross-linking, or

other factors. In the description that follows, the conductive adhesive layer will be taken to be a hydrogel layer for ease of understanding. The principles herein may be applied to essentially any type of electrode that incorporates essentially any type of conductive adhesive or other layer having electrical properties that degrade over time.

[98] Those skilled in the art will understand that electrical current may flow from an electrode's foil layer through the thickness of the electrode's hydrogel layer. In general, an electrode's hydrogel layer may exhibit a thickness of 25 to 50 mils. The electrode **150** may further comprise an insulating cover layer, as well as a lead wire that facilitates coupling to a connector or medical device.

[99] One electrode **150** may be placed or positioned upon the first release layer **110** such that the electrode's hydrogel layer covers one or more of the openings **112** in the release layer **110**. Another electrode **150** may be placed or positioned upon the second release layer **120** in an analogous manner. Placement of electrodes **150** upon the release liner **100** in the manner depicted allows the electrodes' hydrogel layers to contact the moisture-permeable membrane **130** via the openings **112, 122** in the release layers **110, 120**.

[100] Initially, the moisture-permeable membrane **130** may be dry or essentially moisture free throughout one or more bonding, adhesion, lamination, and/or attachment procedures performed during release liner manufacture. In the event that the moisture-permeable membrane **130** remains dry during release liner manufacture, the openings **112, 122** in each release layer **110, 120** may ensure that placement of electrodes **150** upon the release liner **100** results in moisture transfer from each electrode's hydrogel layer into the moisture-permeable membrane **130**. After a period of time, this moisture transfer results in low impedance electrical pathways through the thickness of a given electrode's hydrogel layer, the moisture-permeable membrane **130**, and the thickness of the other electrode's hydrogel layer in regions defined by the release layer openings **112, 122**.

[101] When the electrodes **150** are coupled to a medical or measuring device (not shown), the medical device may measure and/or characterize the electrical pathways between the electrodes' hydrogel layers and the moisture-permeable

membrane **130**. As each electrode's hydrogel layer loses moisture over time, measured impedance increases. Once the measured impedance has reached or surpassed a predetermined value, the electrodes may no longer be in optimal condition, or may be unfit for use. The medical device may provide an indication of electrode status and/or electrode life remaining, and/or indicate that electrode replacement is required, in manners described in detail below.

[102] Placement of electrodes **150** on a release liner **100** having a dry or essentially dry moisture-permeable membrane **130** contributes to hydrogel moisture loss. To prevent or minimize such moisture loss, the moisture-permeable membrane **130** may be prewetted or premoistened in a variety of manners, such as via placement in a high-humidity environment (e.g., 50 – 100% relative humidity) until it has absorbed sufficient moisture to exhibit a low impedance value. When residing between the first and second release layers **110**, **120** prior to electrode placement, the moisture-permeable membrane's impedance may be measured or tested via a set of probes that contact the moisture-permeable membrane **130** through first and second release layers' openings, in a manner well understood by those skilled in the art. The moisture-permeable membrane **130** may alternatively or additionally be moistened using a wet cloth or sponge, or placed in a liquid bath.

[103] Depending upon embodiment and/or implementation details, the moisture-permeable membrane **130** may be bonded, adhered, laminated, and/or otherwise attached to the first release layer **110** but not the second release layer **120**. In such a situation, the adhesion between the hydrogel of an electrode **150** placed upon the second release layer **120** and the moisture-permeable membrane **130** will generally be sufficient to maintain the second release layer **120** in an appropriate position upon the moisture-permeable membrane **130**.

[104] Alternatively, bonding, adhering, laminating, or other moisture-permeable membrane attachment procedures may be omitted for both the first and second release layers **110**, **120**. In such an embodiment, the moisture-permeable membrane **130** is simply placed or situated between the first and second release layers **110**, **120**, after which electrodes **150** are placed or positioned upon the first and second release layers **110**, **120**. In the areas defined by the first and second

release layers' openings **112, 122**, the adhesion between the electrodes' hydrogel layers and the moisture-permeable membrane **130** may be sufficient to appropriately maintain the position of each release layer **110, 120** relative to the moisture-permeable membrane **130**. Such an embodiment can simplify manufacturing processes and reduce production costs.

[105] FIG. 1C is a perspective view of a release liner **170** according to another embodiment of the invention, and a manner of mounting electrodes **150** thereupon. Relative to FIG. 1A, like reference numbers indicate like elements to aid understanding. In one embodiment, the release liner **170** comprises a single release layer **180** having an opening **182** therein, and a moisture-permeable and/or moisture-absorbent membrane **130** covering the opening **182**. The moisture permeable membrane **130** may be bonded, adhered, stitched, and/or otherwise attached to the release layer **180**. In an exemplary embodiment, the moisture-permeable membrane may be heat bonded or ultrasonically bonded to the release liner **170**.

[106] One electrode **150** may be placed or positioned upon the release layer **180** such that the electrode's hydrogel layer covers the release layer's opening **182**. Another electrode **150** may be placed or positioned upon the release layer **180** in an analogous manner. Placement of electrodes **150** upon the release layer **180** allows the electrodes' hydrogel layers to contact the moisture-permeable membrane **130** via the release layer's opening **182**. In the event that the moisture-permeable membrane **130** is dry or essentially moisture free prior to placement of electrodes upon the release layer **180**, moisture transfer from each electrode's hydrogel layer may occur. After a period of time, such moisture transfer results in a low impedance electrical pathway between each electrode's hydrogel layer and the moisture-permeable membrane **130**. The moisture permeable membrane **130** may be premoistened or prewetted as described above to minimize moisture loss from electrodes' hydrogel layers.

[107] When the electrodes **150** are coupled to a medical or measuring device (not shown), the medical device may measure and/or characterize the electrical pathways between the electrodes' hydrogel layers and the moisture-permeable membrane **130** in a manner analogous to that described above.

[108] FIG. 2A is a perspective view of a release liner **200** according to another embodiment of the invention. Relative to FIG. 1A, like reference numbers indicate like elements to aid understanding. In one embodiment, the release liner **200** comprises a foldable release layer or sheet **210** and a moisture-permeable membrane **130**. The foldable release layer **210** comprises a first mounting or release portion, region, or segment **220** having at least one opening **222** therein; a second mounting or release portion, region, or segment **230** having at least one opening **232** therein; and a fold region **240**. In one embodiment, the openings **222**, **232** in the first and second mounting portions **220**, **230** are formed in corresponding positions relative to the fold region **240**, such that when the foldable release layer **210** is folded, bent, or doubled about the fold region **240**, the openings **222**, **232** are essentially coincident.

[109] The foldable release layer **210** may comprise a nonconductive sheet having non-stick properties, and may be formed using silicon-coated paper, polyester, polypropylene, polyethylene, and/or other non-stick materials, in a manner well understood by those skilled in the art. The openings **222**, **232** in the first and second mounting sections **220**, **230** may be cut, stamped, or punched out using conventional techniques.

[110] The moisture-permeable membrane **130** may comprise a non-conductive, moisture-permeable and/or moisture-absorbent material, in a manner analogous to that described above with reference to FIG. 1A. The moisture-permeable membrane **130** may cover an area less than that of the first and/or second mounting portions **220**, **230**, subject to the requirement that it cover or span openings **222**, **232** in each mounting portion **220**, **230** when the foldable release layer **210** is folded. Depending upon embodiment and/or implementation details, the moisture-permeable membrane **130** may be adhered, bonded, laminated, and/or otherwise attached to one, both, or neither of the first and second mounting sections **220**, **230**.

[111] The foldable release layer **210** may be folded, bent, or doubled about the fold region **240** in either direction to surround or encase one or more portions of the moisture-permeable membrane **130**. When folded in such a manner, the

moisture-permeable membrane **130** is exposed in the regions defined by the openings **222, 232** in the first and second mounting portions **220, 230**.

[112] FIG. 2B is a perspective view of electrodes **150** mounted upon the release liner **200** of FIG. 2A. One electrode **150** may be positioned or situated upon an outer surface of the first mounting portion **220**, while another electrode **150** may be positioned upon an outer surface of the second mounting portion **230**. The outer surfaces of the first and second mounting portions **220, 230** together form a single outer surface of the foldable release layer **210**. Thus, both electrodes **150** are mounted upon the same side or surface of the foldable release liner **210**.

[113] In the description herein, release liner mounting portions **220, 230**, such as those described in relation to the release liner **200** of FIGS. 2A and 2B, provide regions or areas upon which electrodes **150** may reside. Electrodes **150** may be readily removed or peeled off of the mounting portions **220, 230**, as the mounting portions **220, 230** comprise non-stick or generally non-stick portions of the release liner **200**.

[114] As with the release liner **100** of FIG. 1A, the moisture-permeable membrane **130** may remain dry or essentially moisture free during release liner manufacture or assembly. In such a situation, a low impedance electrical path may form after electrodes **150** are placed upon the foldable release layer **210** and the electrodes' hydrogel layers transfer moisture into the moisture-permeable membrane **130** in the regions defined by the openings **222, 232** in the first and second mounting portions **220, 230**. Alternatively, the moisture-permeable membrane **130** may be prewetted or premoistened in the manners described above to help minimize hydrogel moisture loss.

[115] Once electrodes **150** are mounted or positioned upon the release liner **200** of FIG. 2A, a medical device to which the electrodes are coupled may test or characterize the electrical path through one electrode's hydrogel layer, the moisture-permeable membrane **130**, and the other electrode's hydrogel layer. As a hydrogel layer loses moisture over time, the medical device may correspondingly measure increasing impedance levels. An impedance value exceeding a given threshold may indicate that the electrodes **150** are not optimally fit for use, or that the

electrodes **150** are unsuitable for use and should be replaced. The medical device may provide an indication of electrode status and/or remaining electrode life, and/or recommend electrode replacement, in manners described in detail below.

[116] FIG. 3A is a layered perspective view of a release liner **300** according

to another embodiment of the invention. Relative to FIG. 1A, like reference elements indicate like elements to aid understanding. The release liner **300** may comprise a first release layer or sheet **310**; a second release layer or sheet **320**; and a moisture-permeable membrane **130**. In contrast to the release liner **100** of FIG. 1A, openings **112**, **122** may not be present in the release layers **310**, **320** of the release liner **300** of FIG. 3A.

[117] Each release layer **310**, **320** may comprise a nonconductive sheet having non-stick properties, and may be implemented using silicon-coated paper, polyester, polypropylene, polyethylene, and/or other non-stick materials, in a manner well understood by those skilled in the art. The moisture-permeable membrane **130** may comprise a non-conductive, moisture-permeable material in the manner described above, which resides between the first and second release layers **310**, **320**.

[118] Portions of the moisture-permeable membrane reside between the release layers **310**, **320**. In one embodiment, the moisture-permeable

membrane **130** overlaps or extends beyond at least one release layer edge or border. Depending upon embodiment and/or implementation details, the moisture-permeable membrane **130** may be adhered, bonded, laminated, and/or otherwise attached to one, both, or neither release layer **310**, **320**, in a manner analogous to that described above with reference to FIG. 1A.

[119] FIG. 3B is a perspective view showing electrodes **150** mounted upon the release liner **300** of FIG. 3A. In the embodiment shown, the electrodes' hydrogel layers **150** contact one or more portions of the moisture-permeable membrane **130** in areas in which the moisture-permeable membrane **130** overlaps or extends beyond release layer boundaries. Thus, portions of the electrodes **150** extend beyond or overlap one or more release layer edges, boundaries, and/or borders. Therefore, the

release layers **310, 320** in such an embodiment may be appropriately sized or scaled relative to the size of the electrodes **150** to facilitate such contact.

[120] As shown in **FIG. 3B**, portions of the electrodes' hydrogel layers contact the moisture-permeable membrane **130**. A low impedance electrical pathway through the thickness of each electrode's hydrogel layer and the moisture-permeable membrane **130** may arise following moisture transfer from hydrogel layers to the moisture-permeable membrane **130**. Alternatively, the moisture-permeable membrane **130** may be prewetted or premoistened to facilitate a low impedance pathway while minimizing hydrogel moisture loss. As with the release liners **100, 200** described above, when electrodes **150** mounted upon the release liner **300** of **FIG. 3A** are coupled to a medical device, the medical device may measure increasing impedance levels over time as the electrodes' hydrogel layers lose moisture. Impedance levels greater than a given threshold or beyond a given range may indicate one or more electrodes **150** are non-optimal or unfit for use. A medical device may provide an indication of electrode condition in a variety of manners described in detail below.

[121] In a manner analogous to that for the embodiments shown in **FIG. 2A** and **FIG. 3A**, a foldable release layer that lacks openings (not shown) may partially enclose or envelop a moisture-permeable membrane **130**, such that the moisture-permeable membrane **130** extends beyond one or more edges of the foldable release layer when so enclosed. When an inner surface of such a foldable release layer surrounds or encases portions of a moisture-permeable membrane **130**, electrodes **150** may be positioned on a common outer surface of the foldable release layer such that the electrodes' hydrogel layers contact exposed portions of the moisture-permeable membrane **130**. This hydrogel to moisture-permeable membrane to hydrogel contact facilitates transfer of electrical signals between electrodes **150**. As in embodiments described above, the moisture-permeable membrane **130** in such an embodiment may or may not be adhered, laminated, or otherwise attached to one or more segments or regions of the foldable release layer. Additionally, the moisture-permeable membrane **130** may be prewetted or premoistened to minimize moisture loss from each electrode's hydrogel layer.

[122] FIG. 4 is a perspective view of a release liner and electrode package **400** according to an embodiment of the invention. The release liner and electrode package **400** may comprise a release liner **404**, electrodes **150** mounted thereupon, and a rigid cartridge **408** in which a release liner **410** and mounted electrodes **150** may be stored prior to use. The release liner **404** may comprise a release layer **410** having an opening **422** therein. The release layer **410** may comprise a nonconductive, non-stick material such as those described above, and the opening **422** may be cut, stamped, or punched out of the release layer **410** via conventional techniques. One electrode **150** may be mounted or positioned upon one side of the release layer **410**, while another electrode **150** may be mounted another side of the release layer **410**, such that each electrode's hydrogel layer covers the release layer's opening **422**. Such electrode mounting may result in hydrogel layer to hydrogel layer contact, thereby facilitating electrical communication between electrodes **150**. In an alternate embodiment, the release layer **410** may include multiple openings **422**, where mounted electrodes **150** may cover some or all of such openings **422**.

[123] The rigid cartridge **408** may comprise a housing or tray **450**, a removable lid **452**, and an electrical interface **460**. The tray **450** and removable lid **452** may comprise plastic or another conventional material, and may store the mounted electrodes **150**. The electrical interface **460** may comprise a connector that facilitates electrical coupling of the electrodes **150** to a medical device. In one embodiment, the rigid cartridge **408** may be implemented in a manner described in U.S. Patent Application Serial No. 09/746,123, entitled CARTRIDGE FOR STORING AN ELECTRODE PAD AND METHODS FOR USING AND MAKING THE CARTRIDGE, filed on December 22, 2000, which is incorporated by reference.

[124] The rigid cartridge **408** facilitates high-reliability sealing of mounted electrodes **150** within an environment that may be characterized by well-defined conditions. In particular, via a conventional technique such as injection molding, the electrical interface **460** may be molded into the tray **450** such that when the lid **452** is sealed upon the tray **450**, moisture transfer into or out of the rigid cartridge **408** is minimized, eliminated, or essentially eliminated. Storage of unused electrodes **150**

within the rigid cartridge **408** may therefore extend electrode shelf life by slowing and/or minimizing moisture loss from the electrodes' hydrogel layers. The rigid cartridge **408** may additionally protect the electrodes **150** contained therein. Such protection may be necessary in the event that the medical device comprises an AED that is deployed or transported in real-world conditions, such as within law enforcement or rescue vehicles.

[125] When electrodes **150** that have been mounted upon the release liner **404** and sealed within the rigid cartridge **408** are coupled to a medical device, the medical device may test and/or characterize the electrical path between the electrical interface **460**, a given electrode's lead wire, the given electrode's conductive foil layer, the given electrode's hydrogel layer, through the release layer's opening **422**, and through the other electrode's hydrogel layer, conductive foil layer, and lead wire back to the electrical interface **460**. In the event that a short or open circuit condition exists, the electrical interface **460**, a lead wire, and/or possibly one or both electrodes **150** may be damaged or defective. In the event that the medical device measures an impedance level or value that exceeds a predetermined threshold or range, the electrodes **150** may be non-optimal or unfit for use. The medical device may provide one or more indications of the condition of the aforementioned electrical path in a variety of manners, as described in detail below.

[126] FIG. 5A is a perspective view of a release liner **500** according to another embodiment of the invention. The release liner **500** may comprise a single release layer or sheet **510**; and a conductive strip **550** positioned, mounted, and/or affixed thereupon. In one embodiment, the release layer **510** may be characterized by a mounting surface **512**, a length **514**, and a width **516**. The release layer **510** comprises a nonconductive sheet having non-stick properties, and may be implemented or fabricated using materials such as those described above with respect to other release liner embodiments. The conductive strip **550** may be characterized by a length **554** and a width **556**, and comprises an electrically conductive material such as a metal foil (e.g., Aluminum or Tin), or an impregnated or sprayed-on metal layer.

[127] In one embodiment, the conductive strip **550** resides upon the release layer's mounting surface **512**. The conductive strip **550** may exhibit a wide range of lengths **554** and/or widths **556**. In the embodiment shown, the conductive strip's length **554** is approximately equal to the length **514** of the release layer **510**, while the conductive strip's width **556** spans a portion of the release layer's width **516**. In general, the conductive strip **550** should be dimensioned to ensure 1) a reliable electrical pathway from one electrode **150** to another exists when the electrodes **150** are placed or mounted in a side-by-side manner upon the release layer **510**; and 2) a sufficient portion of any given electrode's hydrogel layer resides upon the non-stick release layer **510**, thereby facilitating easy removal of electrodes **150** from the release layer **510**. Those skilled in the art will understand that the conductive strip's dimensions **554**, **556** may be impacted by cost and/or manufacturability considerations. Those skilled in the art will further understand that the release layer **510** and/or the conductive strip **550** need not be strictly rectangular, and/or may include one or more nonrectangular portions.

[128] FIG. 5B is a perspective view of electrodes **150** mounted upon the release liner **500** of FIG. 5A. Electrodes **150** may be positioned or mounted upon the mounting surface **512** in a side-by-side manner, such that a portion of each electrode's hydrogel layer electrically contacts the conductive strip **550**. Thus, the conductive strip **550** facilitates current flow between electrodes **150** mounted upon the release liner **500**. When electrodes **150** mounted upon the release liner **500** are coupled to a medical device, the medical device may electrically test or characterize the electrical path from one electrode **150** to the conductive strip **550** to another electrode **150**. A short or open circuit condition may imply a problem with a lead wire, a connector, one or more electrodes **150**, and/or the conductive strip **550**. As electrodes' hydrogel layers lose moisture, the impedance that a medical device may measure along the aforementioned electrical path may increase, indicating that one or more electrodes **150** are non-optimal or unfit for use. As described in detail below, the medical device may perform various operations and/or provide indications of electrode fitness following measurement of an impedance associated with electrodes **150** mounted upon a release liner **500**.

[129] FIG. 6A is a perspective view of another embodiment of a release liner **600** according to an embodiment of the invention. The release liner **600** comprises a foldable release layer or sheet **610** and a conductive strip **650**. The foldable release layer **610** may be characterized by an outer or mounting surface **612**; a length **614**; a width **616**; a first mounting or release portion, region, or segment **620**; a second mounting or release portion, region, or segment **630**; and a fold region **640**. The foldable release layer **610** may be fabricated using a nonconductive, non-stick material in manners previously described. The conductive strip **650** be characterized by a length **654** and a width **656**, and may comprise a material such as Aluminum or Tin. The conductive strip **650** may be positioned, mounted, and/or affixed upon the release layer's mounting surface **612**.

[130] FIG. 6B is a perspective view of electrodes **150** mounted upon the release liner **600** of FIG. 6A. The foldable release layer **610** may be bent, folded, or doubled about the fold region **640** in either direction (i.e., such that the conductive strip **650** is exposed, or such that the conductive strip **650** is enclosed by the release layer **610** and is therefore unexposed), thereby reducing or minimizing the amount of space the release liner **610** and mounted electrodes **150** occupy. Electrodes **150** may be mounted in a side-by-side manner upon the foldable release layer's mounting surface **612**, such that one electrode **150** resides upon the first mounting portion **620** and another electrode resides upon the second mounting portion **630**. When mounted in such a manner, a portion of each electrode's hydrogel layer electrically contacts the conductive strip **650**. Thus, electrical current may flow from one electrode **150** to another via the conductive strip **650**. As with the release liner of FIGS. 5A and 5B, a medical device to which the mounted electrodes **150** are coupled may test or characterize the electrical path between one electrode **150**, the conductive strip **650**, and another electrode **150**. The medical device may provide an indication of electrode fitness based upon such electrical path characterization in manners described below. Those skilled in the art will recognize that the release layer **610** and/or the conductive strip **650** may exhibit a variety of dimensional characteristics, in a manner analogous to that described above with respect to FIG. 5A.

[131] FIG. 7 is a perspective view of a release liner **700** according to another embodiment of the invention, and a manner of mounting electrodes **150** thereupon.

In the embodiment shown, the release liner **700** comprises a conductive strip or band **750** mounted upon a single release layer or sheet **710** having a first and a second indented portion or region **712**, **714**. The release layer **710** comprises a nonconductive, non-stick material constructed in a manner analogous to release layers described above. The indented portions **712**, **714** may be cut, stamped, or punched out of the release layer **710** during manufacture. The conductive band **750** comprises an electrically conductive material such as a metal.

[132] The conductive band **750** may be positioned, mounted, and/or affixed upon or around the release layer **710** within boundaries defined by the release layer's first and second indented portions **712**, **714**. Thus, the conductive band **750** may wrap around the release layer, held in position by borders or edges defined by the release liner's indented portions **712**, **714**. In an alternate embodiment, the conductive band **750** may comprise a first and a second conductive band, which may overlap.

[133] One electrode **150** may be mounted or positioned upon a first side of the release layer **710**, while another electrode **150** may be mounted or positioned upon a second side of the release layer **710**. The conductive band **750** facilitates electrical contact between the electrodes' hydrogel layers. Thus, a medical device to which the mounted electrodes **150** are coupled may test or characterize the electrical path through one electrode **150**, the conductive band **750**, and the other electrode **150**. Those skilled in the art will understand that in alternate embodiments, the release layer may have one or no indented portion **712**, **714**, and/or the conductive band **750** may only partially wrap around the release layer **710**. In such an embodiment, the conductive band **750** may be affixed or adhered to the release layer **710** via conventional techniques. Those skilled in the art will further understand that in an alternate embodiment, the indented portions **712**, **714** may be replaced with protruding portions.

[134] FIG. 8A is a layered perspective view of a release liner **800** according to another embodiment of the invention. The release liner **800** comprises a release

layer or sheet **810** and a backing layer **860**. The release layer **810** may comprise a nonconductive, non-stick sheet having a front or electrode mounting surface **812**; a rear or backing surface **814**; a first opening **822**; and a second opening **832**. The release layer **810** may be manufactured using materials such as those described above, and the openings **822**, **832** therein may be cut, punched, and/or stamped out of such materials via conventional techniques.

[135] The backing layer **860** may comprise an electrically conductive layer positioned, mounted, or affixed upon the release layer's rear surface **814**. When the backing layer **860** is mounted or positioned upon the release layer's rear surface **814**, the nonconductive release layer **810** covers the backing layer **860** except in areas defined by the release layer's openings **822**, **832**. Those skilled in the art will understand that the backing layer **860** need not be the same size as the release layer **810**, as long as the backing layer **860** covers the release layer's openings **822**, **832**. The backing layer **860** may comprise, for example, a metal or foil. The foil may itself be mounted upon or affixed to a substrate or carrier material, such as paper. Alternatively, the backing layer **860** may comprise a conductive adhesive layer, such as a layer of hydrogel, which may reside upon a substrate or carrier material such as paper or plastic.

[136] FIG. 8B is a perspective view of electrodes **150** mounted upon the release liner **800** of FIG. 8A. Electrodes **150** may be mounted upon the release layer's mounting surface **812** in a side-by-side manner, such that one electrode **150** covers the release layer's first opening **822**, and another electrode **150** covers the release layer's second opening **832**. When an electrode **150** covers an opening in the release layer **810**, the electrode's hydrogel layer contacts the conductive backing layer **860** through the opening **822**, **832**. Thus, the openings **822**, **832** facilitate current flow between the electrode's hydrogel layer and the backing layer **860**. Hence, when electrodes **150** reside upon the release liner **800**, electrical current may flow from an electrode **150** covering the first opening **822** into the backing layer **860**, and into an electrode **150** covering the second opening **832**.

[137] In an alternate embodiment, the release layer **810** may comprise two or more separate sheets or electrode mounting or release portions rather than a single

sheet. Each mounting portion may include an opening. Mounting portions upon which electrodes **150** may reside may be positioned upon the conductive backing layer **860** in a variety of manners (electrodes **150** may be positioned upon mounting portions either before or after such mounting portions are situated upon the conductive backing layer **860**). In conjunction with the conductive backing layer **860**, the openings in the mounting portions facilitate electrical communication or signal exchange between electrodes **150**.

[138] In release liner embodiments previously described with reference to **FIGS. 1** through **7**, electrical pathways are defined relative to the thickness of hydrogel layers. Impedance values measured through the thickness of one or more hydrogel layers, however, may coincide with or fall within the same range as impedance values associated with a patient, for example, 50 to 250 Ohms. As a result, a medical device may be unable to determine whether electrodes **150** are attached to a patient's body or residing upon a release liner **100, 200, 300, 400**. Although impedance values measured through hydrogel layer thickness increase as hydrogel layers dry out, even such increased impedance values are likely to overlap the patient impedance range.

[139] Relative to the release liner of **FIGS. 8A** and **8B**, when the backing layer's conductive medium comprises a layer of hydrogel, electrical current may flow through a length of hydrogel defined by a distance between the release layer's first and second openings **822, 832**. The average impedance through the length of a hydrogel layer is much larger than that through the hydrogel layer's thickness. For example, at 70% relative humidity, the average impedance per square through a hydrogel layer's length may be approximately 2 kOhm. This impedance is greater than the patient impedance range by an amount sufficient to ensure that a measured impedance value indicates that electrodes **150** are mounted upon the release liner **800** rather than a patient's body. In addition to the release liner **800** embodiments shown in **FIGS. 8A** and **8B**, other release liner structures that advantageously establish current paths through a length of an electrode's hydrogel layer are described in detail below with reference to **FIGS. 10A, 10B, 11, and 12**.

[140] A medical device to which electrodes **150** mounted upon the release liner **800** of **FIG. 8A** are coupled may test or characterize the electrical pathway defined by one electrode **150**, the backing layer's conductive medium exposed within and extending between the release layer's first and second openings **822**, **832**, and another electrode **150**. A short or open circuit condition may imply a problem with one or more electrodes **150**. As electrodes' hydrogel layers lose moisture, the impedance of the aforementioned electrical path will increase. The impedance of this electrical path will also increase as hydrogel used in the backing layer **860** loses moisture. Upon measuring an impedance level that exceeds a given threshold, the medical device may indicate that the electrodes **150** are non-optimal or no longer fit for use, as further detailed below.

[141] Different hydrogel formulations, as well as identically formulated hydrogels originating from different manufacturing batches, may exhibit different moisture absorption and loss characteristics. Referring again to **FIGS. 8A** and **8B**, in the event that the backing layer **860** comprises a layer of hydrogel originating from a different formulation or manufacturing batch than that of the electrodes **150** mounted upon the release liner **800**, the electrodes' hydrogel layers may donate moisture to or receive moisture from the backing layer's hydrogel. This, in turn, may cause the electrodes' hydrogel layers to undesirably swell or prematurely dry out.

[142] If the backing layer's hydrogel arises from the same manufacturing batch as that of the electrodes **150**, the backing layer's hydrogel will neither donate moisture to or receive moisture from the electrodes' hydrogel layers. Rather, the backing layer's hydrogel may lose moisture to the inside of a package at a rate that is identical or essentially identical to that at which the electrodes **150** lose moisture. The backing layer **860** may therefore provide a moisture reservoir to a package, advantageously enhancing the lifetime of electrodes **150** within the package.

[143] **FIG. 9A** is a perspective view of a release liner **900** according to another embodiment of the invention. The release liner **900** comprises a foldable release layer or sheet **910** and a conductive backing layer **960**. The foldable release layer **910** comprises a nonconductive, non-stick sheet that includes an electrode mounting surface **912**; a backing surface **914**; a first mounting or release portion **920**

having a first opening **922**; a second mounting or release portion **930** having a second opening **932**; and a fold region **940**. The foldable release layer **910** may be manufactured from conventional nonconductive, non-stick materials such as those previously described, where the first and second openings **922**, **932** may be cut, punched, or stamped out of such materials in conventional manners.

[144] The backing layer **960** may comprise a conductive material such as a layer of metal or hydrogel. The foldable release layer **910** may be folded, bent, or doubled in either direction about its fold region **940** such that its backing surface **914** surrounds or encases portions of the backing layer **960**, thereby forming a release layer-backing layer-release layer assembly in which the backing layer **960** is exposed in regions defined by the release layer's first and second openings **922**, **932**.

[145] FIG. 9B is a perspective view showing electrodes **150** mounted upon the release liner **900** of FIG. 9A. One electrode **150** may be mounted upon the release layer's first mounting portion **920**, while another electrode **150** may be mounted upon the release layer's second mounting portion **930**. Thus, the electrodes **150** both reside upon the release layer's mounting surface **912**.

[146] A medical device to which the electrodes **150** are coupled may electrically test or characterize the electrical path through one electrode's hydrogel layer, the release layer's first opening **922**, the conductive medium of the backing layer **960**, the release layer's second opening **932**, and the other electrode's hydrogel layer. A short or open circuit condition may imply a problem with one or more electrodes **150**. As electrodes' hydrogel layers, as well as a hydrogel layer within the conductive backing layer **960** lose moisture, the impedance of the aforementioned electrical path will increase. Upon measuring an impedance level that exceeds a given threshold, the medical device may indicate that the electrodes **150** are non-optimal or no longer fit for use, as further described in detail below.

[147] As described above, release liner structures facilitating electrode characterization via electrical current flow through a given length of hydrogel may enable a medical device to accurately and/or consistently determine whether electrodes **150** are mounted upon the release liner structure or a patient's body.

Additional release liner structures that facilitate electrical characterization of electrodes **150** in this manner are described in detail hereafter.

[148] FIG. 10A is a layered plan view of a release liner **1000** according to another embodiment of the invention. In one embodiment, the release liner **1000** comprises a first release layer or sheet **1020**, a second release layer or sheet **1030**, and an intervening conductive adhesive layer or hydrogel layer **1070**. Each release layer **1020**, **1030** comprises a nonconductive, non-stick material that may be implemented or fabricated using a variety of conventional materials, such as those described above. The first release layer **1020** includes an opening **1022** that is offset or shifted relative to a center point **1024**. Similarly, the second release layer **1030** includes an opening **1032** that is offset or shifted relative to a center point **1034**.

[149] The first and second release layers **1020**, **1030** may be positioned to cover or encase portions of the hydrogel layer **1070**, such that the first and second openings **1022**, **1032** are non-coincident. In such an alignment, the first and second openings **1022**, **1032** are offset with respect to each other relative to any given release layer's center point **1024**, **1034**. When covering or encasing the hydrogel layer **1070**, the first and second release layers **1020**, **1030** may be adhered, laminated, or attached together. Alternatively, adhesion between the release liner's hydrogel layer **1070** and electrodes' hydrogel layers may be sufficient to hold the release liner **1000** together.

[150] FIG. 10B is a perspective view of electrodes **150** mounted upon the release liner of FIG. 10A. One electrode **150** resides upon the first release layer **1020**, while another electrode **150** resides upon the second release layer **1030**. A medical device to which the electrodes **150** are coupled may test or characterize an electrical path through the thickness of one electrode's hydrogel layer in the area spanned by the first opening **1022**; the length of the release liner's hydrogel layer **1070** spanning a distance between the first and second openings **1022**, **1032**; and the thickness of another electrode's hydrogel layer in the area spanned by the second opening **1032**. Since current flows through an electrical path that includes a length of hydrogel significantly larger than the thickness of the electrodes' hydrogel

layers or the release liner's hydrogel layer **1070**, the impedance associated with this electrical path will be significantly greater than typical patient impedance ranges.

[151] The medical device may measure a short or open circuit condition, which may imply dysfunctional or nonoperational electrodes **150**. As the electrodes' hydrogel layers lose moisture, or as the release liner's hydrogel layer **1070** loses moisture, the impedance associated with the electrical path in this embodiment will increase. The medical device may subsequently determine that the electrodes **150** are non-optimal or unfit for use, and provide an indication of such in manners detailed below.

[152] FIG. **11A** is a perspective view of a release liner **1100** according to another embodiment of the invention. In one embodiment, the release liner **1100** comprises a foldable release layer or sheet **1110** and a hydrogel layer **1170**. The foldable release layer **1110** may comprise a nonconductive, non-stick sheet that includes an electrode mounting surface **1112**; a rear surface **1114**; a first mounting or release portion **1120** having a first opening **1122** offset relative to a midpoint **1124** within the first mounting portion **1120**; a second mounting or release portion **1130** having a second opening **1132** offset relative to a midpoint within the second mounting portion **1130**; and a fold region **1140**. The foldable release layer **1110** may be fabricated from conventional materials such as those described above, where the first and second openings **1122**, **1132** may be cut, punched, and/or stamped out in conventional manners. In an alternate embodiment, the first and/or second openings **1122**, **1132** may respectively comprise a first and/or a second set of openings.

[153] The foldable release layer **1110** may be folded, bent, or doubled about its fold region **1140** such that its rear surface **1114** surrounds or encases portions of the hydrogel layer **1170**. The hydrogel layer **1170** may be exposed via the first and second openings **1122**, **1132** within the first and second mounting portions **1120**, **1130**, respectively. When the release layer **1110** is folded and encases the hydrogel layer **1170**, the first and second openings **1122**, **1132** are non-coincident or offset relative to each other, such that they are separated by a predetermined or as-manufactured length or distance. This separation distance

ensures that when electrodes **150** are mounted upon the release liner **1100** and coupled to a medical device, electrical current may travel through a given length of the hydrogel layer **1170**, where this length is significantly greater than the hydrogel layer's thickness. As a result, the electrical path provided by the release liner of

- 5 **FIG. 11A** may exhibit an impedance level significantly greater than typical patient transthoracic impedance levels.

[154] **FIG. 11B** is a perspective view of electrodes **150** mounted upon the release liner **1100** of **FIG. 11A**. Electrodes **150** mounted upon this release liner **1100** may be tested and/or characterized in manners analogous to those described above
10 for other release liner embodiments.

[155] Electrodes themselves may be designed such that current flow within the electrode may occur through a given length of the electrode's hydrogel layer when the electrodes are mounted upon a release liner. Various electrode
15 embodiments that may be characterized by current flow through portions of a hydrogel layer's length are described in detail hereafter.

[156] **FIG. 12A** is a cross sectional view of an electrode **1200** according to an embodiment of the invention. **FIG. 12B** is a plan view of the electrode **1200** of **FIG. 12A**. In the embodiment shown, the electrode **1200** comprises a conductive
20 adhesive material, gel layer, or hydrogel layer **1210**; a conductive or foil layer **1220** having at least one opening or void **1222** therein; an insulating or dielectric layer **1230**; and a lead wire **1240**. Each element **1210**, **1220**, **1230**, **1240** within the electrode **1200** may be implemented using conventional materials. The hydrogel layer **1210** interfaces the electrode **1200** to a patient's body or a release liner. The foil layer **1220** resides upon the hydrogel layer **1210**, and the insulating layer **1230**
25 resides upon the foil layer **1220**. Finally, the lead wire **1240** is coupled to the foil layer **1220**, and may be covered with an insulating material in a manner well understood by those skilled in the art.

[157] Each void **1222** may be cut, stamped, or punched out of the conductive foil layer **1220** in a conventional manner. Furthermore, each void **1222** may be
30 positioned at a given location that corresponds to an area in which electrical contact with a conductive region, area, section, and/or element of an appropriate type of

release liner is desired. The presence of a void **1222** in the foil layer **1220** may affect the manner in which electrical current may flow through or within the electrode **1200** when the electrode **1200** is mounted upon a patient's body.

[158] **FIG. 13A** is a graph of exemplary current density relative to lateral position for a conventional electrode mounted upon a patient's body. Those skilled in the art will understand that current flows more easily between an electrode and a patient's body near the electrode's edges. As one moves from an interior region toward an outer edge or border of the electrode's foil layer, current density increases and peaks.

[159] **FIG. 13B** is a graph showing exemplary shock current density relative to lateral position beneath elements of an electrode **1200** of **FIG. 12A** when the electrode **1200** is mounted upon a patient's body. Within a region defined by a void **1222**, current density drops to a minimum value relative to its value beneath the foil layer **1220**. At a foil layer edge or boundary, current density exhibits a peak. The presence of a void **1222** provides an additional foil layer edge or boundary at which a current density peak may occur. Those skilled in the art will understand that as a result of such current density peaks, the presence of one or more properly positioned voids **1222** in the foil layer **1220** need not increase, and may decrease, the effective shock impedance of the electrode **1200**. Those skilled in the art will thus understand that the areas under the curves shown in **FIGS. 13A** and **13B** may be identical or essentially identical. Alternatively, the area under the curve shown in **FIG. 13B** may be greater than that under the curve shown in **FIG. 13A**.

[160] The presence of a void **1222** in an electrode's foil layer **1220** may also affect the manner in which electrical current may flow through or within the electrode **1200** when the electrode **1200** is mounted upon a release liner. **FIG. 14A** is a perspective view of two voided electrodes **1200** of **FIG. 12A** mounted upon a release liner **1400** according to another embodiment of the invention. **FIG. 14B** is a cross sectional view of the voided electrodes **1200** mounted upon the release liner **1400** of **FIG. 14A**. The release liner **1400** may comprise a nonconductive, non-stick release layer **1410** having an opening **1422** therein. The release layer **1410** may be implemented using conventional materials such as those previously

described, and the opening **1422** may be cut, stamped, or punched out of the release layer **1410** via conventional techniques.

[161] The release layer's opening **1422** may be smaller than the voids **1222** in the electrodes' conductive foil layers **1220**. One voided electrode **1200** may be mounted upon one side of the release layer **1410**, while another electrode **1200** may be mounted upon the release layer's opposite side, such that the void **1222** in each electrode's conductive foil layer **1220** surrounds the release layer's opening **1422**. The release layer's opening **1422** facilitates hydrogel layer **1210** to hydrogel layer **1210** contact within areas defined by each electrode's void **1222**.

[162] The presence of a void **1222** may ensure that electrical current flow involves a hydrogel layer's length and/or width in addition to the hydrogel layer's thickness. That is, current flow may include or be decomposed into lateral or transverse components that are parallel or essentially parallel to a plane defined by the interface between the electrode's hydrogel layer **1210** and the conductive foil layer **1220**. When voided electrodes **1200** mounted upon a release liner **1400** are coupled to a medical or measuring device, electrical current may flow from an edge of a given electrode's conductive foil layer **1220** that defines a void's boundary or border, through the given electrode's hydrogel layer **1210** and to the release liner opening **1422** along a path that includes transverse or lateral components, and into and through the other electrode **1200** in a corresponding manner. In other words, electrical current may flow from one electrode **1200** to another along a current path that includes transverse or lateral components through each electrode's hydrogel layer **1210**. Exemplary current paths that include transverse or lateral components are indicated in **FIG. 14B** via curved arrows.

[163] Electrical current may travel a greater distance along a current path that involves transverse components than along a current path defined solely by a hydrogel layer's thickness. Also, bulk impedance values may be larger and/or more readily measured over a longer current path than a shorter current path. As a result, an electrical path that includes or involves transverse components or a length of an electrode's hydrogel layer **1210** between a foil layer/void boundary and a release liner opening **1422** may be characterized by a higher impedance than an electrical

path defined by a hydrogel layer's thickness. This, in turn, may ensure that the impedance level corresponding to electrodes **1200** appropriately mounted or positioned upon a release liner **1400** is greater than typical patient impedance levels. Additionally, electrodes **1200** that may be characterized via measurements involving transverse current components (e.g., electrodes **1200** that incorporate one or more voids **1222**) may exhibit enhanced response to impedance changes resulting from hydrogel layer moisture loss.

[164] As a result of the foregoing, electrodes **1200** having one or more voids **1222** incorporated therein and which are mounted upon a release liner **1400** may exhibit a packaged or mounted impedance level that is greater or significantly greater than typical patient impedance levels, even for electrodes **1200** that are new, essentially new, and/or in excellent, good, and/or acceptable operating condition. As the condition of one or more such electrodes **1200** deteriorates over time, a packaged impedance measurement may provide a particularly sensitive indication of deterioration, as a corresponding measured impedance may exhibit a large increase over time in response to such deterioration.

[165] The size or area associated with an electrode's void **1222** relative to 1) the size, area, and/or position of a release liner's opening **1422**; and/or 2) the thickness of the electrode's hydrogel layer **1210** may affect or determine an extent to which transverse components contribute to electrical current flow. Larger transverse contributions to electrical current flow result in larger measured impedance values. A hydrogel layer **1210** may be characterized by a thickness H. A boundary or edge separation distance between a void **1222** and a release liner opening **1422** may be characterized by a distance L, as shown in FIG. 14B. In one embodiment, to ensure sufficient transverse or lateral contributions to electrical current flow between electrodes **1200** mounted upon a release liner **1400**, the ratio L/H should be significantly greater than 1.

[166] The area associated with a given void **1222** may be larger than that associated with a release liner opening **1422** over which the void **1222** is positioned. In an exemplary embodiment, a void **1222** may have an area approximately **300%** greater than a release liner opening **1422**. Such an area relationship may aid

manufacturability by providing a positional tolerance during electrode mounting procedures. Those skilled in the art will understand that the voided electrodes **1200** may have differently sized and/or differently shaped voids, which may further influence the manner in which electrical current may laterally flow through portions of a hydrogel layer. In addition, one or more voids may be present in one electrode **1200**, while another electrode lacks voids.

[167] A medical device to which voided electrodes **1200** mounted to a release liner **1400** are coupled may reliably determine whether the voided electrodes **1200** are mounted upon the release liner **1400** or a patient's body. A medical or measuring device may determine that a short or open circuit condition exists along or within the aforementioned electrical path, in which case the electrical path and/or one or more electrodes **1200** may be damaged or defective. The medical or measuring device may also determine an electrode condition or fitness level based upon an impedance measurement. As indicated above, impedance measurements involving transverse or lateral current paths may be particularly sensitive to changes in hydrogel layer moisture content. In the event that an impedance measurement result exceeds a given threshold or range, the medical or measuring device may provide an indication that the electrodes **1200** may be non-optimal or unfit for use, in manners described in detail below.

[168] FIG. 15 is a plan view of the electrode **1200** of FIG. 12A and a conventional electrode **150** mounted upon the release liner of FIG. 8A. The voided electrode **1200** is mounted or oriented such that a void **1222** therein surrounds the release liner's first opening **822**, while the conventional electrode **150** is positioned such that it covers or overlaps the release liner's second opening **832**. Those skilled in the art will understand that the conventional electrode **150** may be replaced with a voided electrode **1200**, **1250** in an alternate embodiment. In an embodiment having an electrode **1250** with multiple voids **1222**, **1224**, the release liner **800** may include an appropriate set of openings corresponding to each such void **1222**, **1224**.

[169] A medical device to which the electrodes **1200**, **150** are coupled may test or characterize the electrical path laterally through a length of the voided electrode's hydrogel layer **1210**, through the release liner's conductive backing

layer **860**, and through the hydrogel thickness within the conventional electrode **150**. A measured impedance level that exceeds a given threshold and/or falls outside a particular range may indicate that one or more electrodes **1200**, **150** mounted upon the release liner **800** are non-optimal or unfit for use. The medical device may provide one or more indications of electrode condition or fitness in manners described in detail below.

[170] As described above, any given void **1222**, **1224** may affect the manner in which current flow occurs through and/or within an electrode **1200**, **1250**. The presence of a void **1222**, **1224** may result in transverse or lateral current flow through a portion of an electrode's hydrogel layer **1210**. For example, when an electrode **1200** is mounted upon a nonconductive release layer such that a void **1222**, **1224** surrounds a release layer opening that facilitates access to a conductive medium, a direct electrical path from a foil layer **1220** through the thickness of the hydrogel layer **1210** to the conductive medium may not exist. As a result, transverse current flow may occur. As previously indicated, an electrode **1200** may include multiple voids **1222**, which may be shaped and/or positioned in a variety of manners relative to each other.

[171] **FIG. 12C** is a plan view of an electrode **1250** according to another embodiment of the invention. Relative to **FIGS. 12A** and **12B**, like reference numbers indicate like elements for ease of understanding. In the embodiment shown, the electrode **1250** comprises a hydrogel layer **1210**; a conductive or foil layer **1220** having a void **1222** and a recess **1224**; a dielectric layer **1230**; and a lead wire **1240**. Each of the hydrogel layer **1210**, the foil layer **1220**, the dielectric layer **1230**, and the lead wire **1240** may be implemented using conventional materials.

[172] The void **1222** may comprise a generally circular, elliptical, or otherwise shaped opening that is generally disposed or positioned within a central region or area of the foil layer **1220**. The recess **1224** may comprise an opening and/or open region that extends to an outer edge or boundary of the foil layer **1220**. Each void and/or recess **1222**, **1224** may be positioned over a corresponding opening in a release liner. In accordance with various embodiments, the voids **1222** and/or

recesses **1224** detailed above may be shaped and/or positioned differently. Additionally, any given electrode embodiment may have additional or fewer voids **1222** and/or recesses **1224**.

[173] The presence of an insulating material may affect electrical current flow between electrodes mounted upon a release liner in a manner that is identical or essentially identical to that described above relative to voids **1222**, as described in detail hereafter.

[174] FIG. **12D** is a cross sectional view of an electrode **1260** according to another embodiment of the invention. FIG. **12E** is a plan view of the electrode **1260** of FIG. **12D**. Relative to FIGS. **12A**, **12B**, and **12C**, like reference numbers indicate like elements. The electrode **1260** may comprise a hydrogel layer **1210**; a conductive or foil layer **1220**; an insulating or dielectric layer **1230**; and a lead wire **1240**, each of which may be implemented using conventional materials. The electrode **1260** further comprises a set of insulating or nonconductive internal patches or swatches **1226**. While FIGS. **12D** and **12E** show an embodiment that includes a single internal swatch **1226**, additional internal swatches **1226** may be present in alternate embodiments. Those skilled in the art will also understand that in alternate embodiments, an electrode may include one or more voids **1222**, **1224** instead of or in addition to one or more internal swatches **1226**.

[175] Any given internal swatch **1226** may comprise an insulating material such as polyethylene. Each internal swatch **1226** may reside between the hydrogel layer **1210** and the conductive foil layer **1220**. An internal swatch **1226** may be positioned at a given location that corresponds to an area in which electrical contact with a conductive region, area, section, and/or element of a release liner or another electrode is desired. Because the internal swatch **1226** is nonconductive, its presence affects the manner in which current may flow through and/or within the electrode **1260**, in a manner analogous to that described above for voids **1222**.

[176] FIG. **16** is a plan view showing electrodes **1260** of FIG. **12D** mounted upon the release liner **800** of FIG. **8A**. One electrode **1260** may be positioned or oriented such that its internal swatch **1226** overlaps or surrounds the release liner's first opening **822**, while another electrode **1260** may be positioned or mounted such

that its internal switch **1226** overlaps the release liner's second opening **832**. A direct electrical path from any given electrode's foil layer **1220** through the thickness of the electrode's hydrogel layer **1210** and into the release liner's conductive backing layer **860** via the first or second opening **822, 832** may not exist due to the presence of the internal switches **1226**. Thus, the presence of an internal switch **1226** may result in lateral or transverse current flow through a length of an electrode's hydrogel layer **1210**. Such current flow originates from a foil layer **1220** along a boundary or interface defined by an intersection of the foil layer's area and the area of the internal switch **1226**, and laterally extends to or past a boundary or interface defined by the area of an appropriate release liner opening **822, 832**. Those skilled in the art will understand that electrodes **1260** incorporating one or more internal switches **1226** therein may be mounted upon other release liner types, such as the release liner **1400** of FIG. **14A**.

[177] A medical device to which the electrodes **1260** are coupled may test or characterize the electrical path through a length of each electrode's hydrogel layer **1210** and through the release liner's conductive backing layer **860** via the first and second release liner openings **822, 832**. A measured impedance level that exceeds a given threshold and/or falls outside a particular range may indicate that one or more electrodes **1260** mounted upon the release liner **800** are non-optimal or unfit for use. The medical device may provide one or more indications of electrode condition or fitness in manners described in detail below.

[178] Those skilled in the art will understand that in alternate embodiments, essentially any of the electrodes **1200, 1250, 1260** of FIGS. **12A, 12B, 12C, 12D, and 12E** may be mounted upon various types of release liners in conjunction with identical, similar, and/or conventional electrodes **150**. Use of voided electrodes **1200, 1250** and/or electrodes **1260** that include an internal switch **1226** may require release liner embodiments that ensure no overlap between portions of such electrodes' foil layers and a conductive region or medium associated with the release liner exists (i.e., release liner embodiments that ensure a significant amount of transverse current flow through a length of an electrode's hydrogel layer **1210**).

[179] Other electrode designs may facilitate electrical path characterization while mounted upon a release liner, in conjunction with determination of whether electrodes are mounted upon the release liner or a patient's body. **FIG. 17** is a cross sectional view of an electrode **1700** according to another embodiment of the invention. The electrode **1700** may comprise a conductive adhesive material, conductive gel layer or hydrogel layer **1710**, a foil layer **1720**, an insulating layer **1730**, and a first lead wire **1740**, each of which may be implemented using conventional materials. The electrode **1700** further comprises a sonomicrometer **1770** coupled to a second lead wire **1780**.

[180] The sonomicrometer **1770** comprises a piezoelectric transducer capable of transmitting and/or receiving ultrasonic signals (i.e., sound signals having frequencies greater than or equal to 1 MHz). The sonomicrometer **1770** is positioned upon or partially embedded within the hydrogel layer **1710**. A sonomicrometer **1770** may serve as an ultrasonic transmitter and/or an ultrasonic receiver. A sonomicrometer **1770** suitable for incorporation into an electrode **1700** may comprise a piezoelectric transducer available from Sonometrics Corporation (www.sonometrics.com). As described in detail hereafter, sonomicrometers **1770** incorporated into a group of electrodes **1700** may facilitate measurement of a separation distance between electrodes **1700**, thereby determining or indicating whether electrodes **1700** are mounted upon a release liner or a patient's body.

[181] **FIG. 18** is a perspective view of electrodes **1700** of **FIG. 17** mounted upon the release liner **1400** of **FIG. 14A** in accordance with an embodiment of the invention. Relative to **FIGS. 14A** and **17**, like reference numbers indicate like elements. One electrode **1700** may be mounted upon one side of the release layer **1410**, while another electrode **1700** may be mounted upon the release layer's opposite side. The release layer's opening **1422** facilitates hydrogel layer **1710** to hydrogel layer **1710** contact, thereby providing for direct electrical communication between electrodes **1700**.

[182] The first and second lead wires **1740**, **1780** of each electrode **1700** may be coupled to a medical device. The medical device may electrically test or characterize the electrical path through one electrode's hydrogel layer **1710**, through

the release layer's opening **1422**, and into the other electrode's hydrogel layer **1710**. In the event that the medical device measures a short or open circuit condition, one or more electrodes **1700**, lead wires **1740**, and/or connectors that couple the electrodes **1700** to the medical device may be defective.

- 5 **[183]** As the electrodes' hydrogel layers **1710** lose moisture over time, an impedance level or value associated therewith may increase. If the medical device measures an impedance value that exceeds a particular threshold or range, one or both electrodes **1700** may be non-optimal or unfit for use. The medical device may perform one or more operations and/or provide one or more indications of electrode
- 10 condition in manners described in detail below.

- [184]** The medical device may issue a separation measurement signal to one electrode's sonomicrometer **1770** via a second lead wire **1780**. In response, the sonomicrometer **1770** may issue or generate an ultrasonic pulse, which may travel 1) through the signal generating electrode's hydrogel layer **1710**; 2) through the release
- 15 layer **1410** and/or the release layer's opening **1422**; 3) and into the other electrode's hydrogel layer **1710**, whereupon it may be detected and/or received by a receiving sonomicrometer **1770**. The receiving sonomicrometer **1770** may issue a reception signal to the medical device in response to detection of the ultrasonic pulse.

- [185]** The medical device may calculate or determine a separation distance
- 20 between sonomicrometers **1770** based upon the time delay between issuance of the separation measurement signal and receipt of the reception signal, in a manner readily understood by those skilled in the art. Based upon the separation distance, the medical device may determine whether the electrodes **1700** are mounted upon the release liner **1400**. A separation distance smaller than a given threshold
- 25 distance, for example, one inch, provides an indication that the electrodes **1700** are mounted upon the release liner **1400** rather than a patient's body. In an alternate embodiment, a release liner **1400** itself may include a sonomicrometer **1770**.

- [186]** In the event that the medical device determines, calculates, or measures a separation distance significantly greater than that associated with
- 30 electrodes **1700** mounted or packaged upon a release liner **1400**, the medical device may determine that the electrodes **1700** are mounted upon a patient's body. Based

upon a measured or determined separation distance, the medical device may further determine whether the electrodes **1700** are properly positioned upon the patient's body. For example, the medical device may determine that the electrodes **1700** are positioned too close together, and provide a message to a medical device operator indicating such and/or requesting electrode repositioning. The medical device may further adjust, modify, or tailor a signal exchange sequence with the patient based upon a measured or determined electrode separation distance. For example, a medical device such as an AED may determine that a measured electrode separation distance indicates that the electrodes **1700** are mounted upon a large patient, and increase one or more shock energies accordingly.

[187] In an alternate electrode embodiment, an electrode's foil layer **1720** may include an opening therein (not shown), in a manner analogous to that described above with reference to **FIGS. 12A** through **12C**. The sonomicrometer **1770** may be situated or positioned within such an opening, in which case an ultrasonic signal may travel directly through one electrode's hydrogel layer **1710** into another electrode's hydrogel layer **1710** via the opening without experiencing significant signal attenuation due to the release layer **1410**.

[188] A wide variety of electrode/release liner configurations in addition those disclosed above may exist. **FIG. 19** is a perspective view of voided electrodes **1250** of **FIG. 12C** and a conventional electrode **150** mounted upon a release liner **1900** in accordance with another embodiment of the invention. The release liner **1900** may comprise a foldable release layer **1910** and a conductive backing layer **1960**. The foldable release layer **1910** may comprise a nonconductive, non-stick material having a first mounting or release portion **1920**, a second mounting or release portion **1930**, and a third mounting or release portion **1936**. The first, second, and third mounting portions **1920**, **1930**, **1936** may respectively include first a set of openings **1922**, a second set of openings **1932**, and a third set of openings **1938** therein. The first and second mounting portions **1920**, **1930** may be separated by a first fold region **1940**, while the second and third mounting portions **1930**, **1936** may be separated by a second fold region **1942**. The foldable release layer **1910** may be implemented using conventional materials, such as those described above, and the first, second, and/or

third sets of openings **1922, 1932, 1938** may be cut, stamped, and/or punched out of such materials in conventional manners.

[189] The conductive backing layer **1960** may comprise a foldable or bendable sheet or layer of conductive material, such as an Aluminum or Tin foil layer.

5 Depending upon embodiment and/or implementation details, the conductive backing layer **1960** may be adhered, laminated, and/or otherwise attached to the release layer **1910**. Additionally or alternatively, the conductive backing layer **1960** may be held in position via adhesion to hydrogel in regions in which the first, second and/or third sets of release layer openings **1922, 1932, 1938** expose the backing layer **1960**
10 to electrodes **1250, 150** mounted upon the release layer **1910**.

[190] Electrodes **1250, 150** may be mounted upon each of the foldable release layer's mounting portions **1920, 1930, 1936**, for example, in the manner shown in **FIG. 19**. Electrodes **1250, 150** mounted in such a manner reside upon a single side of the foldable release layer **1910**; that is, electrodes **1250, 150** so
15 mounted reside upon the same surface of the foldable release layer **1910**. The foldable release layer **1910** may be folded, bent, or doubled about one or more fold regions **1940, 1942**.

[191] A medical device to which the electrodes **1250** are coupled may test and/or characterize the electrical path between any pair of electrodes **1250, 150**
20 and/or all electrodes **1250, 150** in a manner analogous to that described above. The medical device may provide one or more indications of electrical path and/or electrode condition in manners described in detail below.

[192] Those skilled in the art will understand that other electrode/release liner configurations may include conventional electrodes **150**; voided
25 electrodes **1200, 1250** in accordance with **FIGS. 12A, 12B, and 12C**; electrodes **1260** having one or more swatches **1226** incorporated therein in a manner analogous to that described above with reference to **FIGS. 12D and 12E**; sonomicrometer electrodes **1700**; and/or other electrodes. Release liners upon which such electrodes may be mounted may include an appropriate set of openings
30 to facilitate electrical communication between electrodes in manners analogous to those described above.

[193] The release liner and/or electrode embodiments described above facilitate electrical characterization of packaged electrodes via electrical contact between electrodes. Release liner and/or electrode embodiments that facilitate such characterization via measurements that may not rely upon electrode to electrode contact are considered in detail hereafter.

[194] FIG. 20 is a perspective view of electrodes **150** mounted upon a release liner **2000** in accordance with an embodiment of the invention. The release liner **2000** may comprise a release layer **2010** having two sides and characterized by nonconductive and non-stick properties. The release layer **2010** may be characterized by a known thickness and dielectric constant, may be implemented using a variety of conventional materials including those described above.

[195] One electrode **150** may be positioned or mounted upon one side of the release layer **2010**, while another electrode may be analogously positioned upon the release layer's other side. For a given electrode **150**, the effective electrical contact area to the release layer **2010** may correspond to the area spanned by the electrode's hydrogel layer. Alternatively, the effective electrical contact area to the release layer **2010** may be a function of the area of the electrode's hydrogel layer relative to that of the electrode's foil layer.

[196] The electrical contact area associated with each electrode **150**, as separated by a release layer having a known thickness and dielectric constant, forms a type of parallel plate capacitor. A medical device coupled to electrodes **150** mounted upon a release liner **2000** in the manner shown in FIG. 20 may therefore measure, determine, or calculate a corresponding capacitance value. In one embodiment, the thickness and capacitance associated with the release liner are approximately 5 mils and 1 nF, respectively. The effective electrical contact area may be approximately **100** square centimeters.

[197] If the capacitance value is above or below a predetermined or expected range, a short or open circuit condition may exist, possibly indicating a damaged or defective electrical path, possibly arising from a problem with an electrode **150**, wiring, and/or a connector. In such a situation, the medical device may provide an

indication that the packaged electrodes **150** are unfit for use, possibly in manners described in detail below.

[198] A medical or measuring device may alternatively or additionally perform a complex impedance measurement upon electrodes **150** mounted upon a release liner **2000** as shown in **FIG. 20**. A complex impedance may be characterized by a real impedance R (i.e., a resistance); and an imaginary impedance X (i.e., a reactance in the context of the present invention). When electrodes **150** are mounted upon a release liner **2000**, a real impedance may correspond to hydrogel layer moisture content, and an imaginary impedance may correspond to a capacitance within the electrode/release liner configuration. As the electrodes' hydrogel layers lose moisture over time, the medical or measuring device may measure a corresponding increase in a real impedance R . The medical or measuring device may include temperature measurement and/or compensation circuitry or elements to account for manners in which measured impedance levels may vary as a function of temperature. If the medical or measuring device determines that a temperature compensated real impedance value exceeds a given threshold value and/or falls outside an acceptable range, one or more electrode's hydrogel layers may have dried out to an extent that such electrodes **150** are no longer optimal or fit for use. The medical or measuring device may provide an indication of such, possibly in manners described in detail below.

[199] The magnitude of a real impedance R relative to that of an imaginary impedance X may determine an extent to which a medical device can detect or determine a hydrogel layer's condition. In the embodiment shown in **FIG. 20**, an imaginary impedance X may dominate complex impedance measurements. Thus, small changes in a real impedance R may be difficult to detect, making accurate and/or detailed characterization of electrode hydrogel layer condition correspondingly difficult.

[200] Electrode and/or release liner structure may have a significant impact upon the magnitude of a real impedance R relative to that of an associated imaginary impedance X . In particular, release liner and/or electrode structures that minimize an imaginary impedance X and/or maximize a real impedance R may facilitate

determination of more detailed information about hydrogel layer condition. Release liner and/or electrode embodiments directed toward maximizing detectability of changing hydrogel layer conditions are described in detail hereafter.

[201] **FIG. 21A** is a plan view of a release liner **2100** according to an embodiment of the invention. In the embodiment shown, the release liner **2100** comprises a two-sided release layer **2110** having an opening **2122** therein; and an insulating swatch or patch **2126** that covers or fills the opening **2122**. The release layer **2110** may comprise a conventional nonconductive, non-stick material, in a manner described above. The insulating swatch **2126** may comprise a thin layer of nonconductive material characterized by a high dielectric constant. The swatch **2126** may be implemented, for example, using Polyvinyl Chloride (PVC), which typically exhibits a dielectric constant ranging between 4.8 and 8; Polyvinidene fluoride (PVDF), which may exhibit a dielectric constant ranging between 8 and 10; a ceramic material such as BaTiO₃, which may exhibit a dielectric constant ranging between 350 and 6500; and/or other materials. The thickness of the swatch **2126** in any given implemented may depend upon manufacturing and/or material handling considerations. Polymeric swatches **2126** may comprise one or more film-based layers, and may have a thickness of 1 mil or less. Ceramic-based swatches **2126** may exhibit a thickness range, for example, between 2 and 10 mils.

[202] **FIG. 21B** is a perspective view of electrodes **150** mounted upon the release liner **2100** of **FIG. 21A**. One electrode **150** may be positioned upon one side of the release layer **2110**, while the other electrode **150** may be positioned upon the release layer's other side, forming an electrode **150** to release liner **2100** to electrode **150** assembly **2102**. A medical or measurement device to which the electrodes **150** are coupled may perform a complex impedance measurement upon the assembly **2102**.

[203] **FIG. 21C** is a cross sectional view of the electrode to release liner to electrode assembly **2102** of **FIG. 21B**. **FIG. 21D** is an equivalent circuit **2190** corresponding to or modeling the assembly **2102** of **FIG. 21B**. The equivalent circuit **2190** may be characterized by a first circuit branch **2192** in parallel with a second circuit branch **2194**. The first circuit branch **2192** includes a first resistance

R1 and a first capacitance C1, and may be characterized by a first impedance Z1. Impedance Z1 may be decomposed or represented as $R1 + X1$, where X1 is a reactance associated with capacitance C1, equal to $1/(j\omega C1)$. The second circuit branch **2194** includes a second resistance R2 and a second capacitance C2, and may be characterized by a second impedance Z2. Impedance Z2 may be represented as $R2 + X2$, where X2 is a reactance associated with capacitance C2, equal to $1/(j\omega C2)$.

[204] The first circuit branch **2192** may correspond to a displacement current path that excludes an area in which the swatch **2126** covers, fills, overlaps, and/or blocks the release layer's opening **2122**. That is, the first circuit branch **2192** may correspond to a displacement current path outside a boundary defined by an area in which the swatch **2126** covers the opening **2122**. This displacement current path may exist through one electrode's conductive foil and hydrogel layers, the release layer **2110** (and possibly portions of the swatch **2126** that extend beyond a boundary defined by the opening **2122**), and the other electrode's conductive foil and hydrogel layers. Thus, within the first circuit branch **2192**, resistance R1 may correspond to an effective conductive and hydrogel layer resistance within the electrodes **150** in areas excluding those in which the swatch **2126** covers the opening **2122**. Similarly, capacitance C1 may correspond to an effective capacitance of the release layer **2110** in areas excluding those in which the swatch **2126** covers the opening **2122**.

[205] The second circuit branch **2194** may correspond to a displacement current path through areas or portions of the swatch **2126** that cover or fill the opening **2122**. That is, the second circuit branch **2194** may correspond to the displacement current path from one electrode's conductive foil and hydrogel layers in an area in which the swatch **2126** covers the opening **2122**; through the swatch **2126** where it covers or fills the opening **2122**; and into the other electrode's conductive and hydrogel layers in this area. Thus, within the second circuit branch **2194**, resistance R2 may correspond to an effective conductive and hydrogel layer resistance associated with the electrodes **150** in an area of the swatch **2126** where it covers the opening **2122**, while capacitance C2 may correspond to an effective

capacitance associated with the swatch **2126** in or over an area defined by the opening **2122**.

[206] An effective impedance Z_{eff} may be defined as $((1/Z1) + (1/Z2))^{-1}$, in a manner readily understood by those skilled in the art. Those skilled in the art will also understand that an effective current I_{eff} may thus vary in accordance with $((1/Z1) + (1/Z2))$, or $(1/(R1 + X1) + 1/(R2 + X2))$. For electrodes **150** in good condition, the values of resistances $R1$ and $R2$ may generally be small. Capacitance $C2$ may be significantly larger than capacitance $C1$, and hence reactance $X2$ is correspondingly smaller than reactance $X1$. Additionally, reactance $X2$ may be sufficiently small that it does not overwhelm or dominate the term $1/(R2 + X2)$. Neither $X1$ nor $X2$ generally experience significant changes over time. Hence, changes in resistance $R2$ over time, which may correspond to changes in hydrogel layer moisture content, may noticeably affect the complex impedance of the assembly **2102**. Other electrode/release liner configurations or embodiments in which changes in hydrogel layer properties may significantly affect complex impedance measurements are described in detail hereafter.

[207] FIG. **22A** is a perspective view of a voided electrode **1200** of FIG. **12A** and a conventional electrode **150** mounted upon the release liner **2100** of FIG. **21A**. Relative to FIGS. **12A** and **21A**, like reference numbers indicate like elements. The voided electrode **1200** may be mounted upon one side of the release layer **2110**, while the conventional electrode **150** may be mounted upon the release layer's other side, forming a voided electrode **1200** to release liner **2100** to conventional electrode **150** assembly **2102**. The voided electrode **1200** may be mounted or positioned such that its void **1222** surrounds or encompasses at least a portion of the release liner's swatch **2126**, namely, that portion of the swatch **2126** that covers, fills, and/or overlaps the release layer's opening **2122**. Those skilled in the art will understand that the area occupied by the void **1222** may be larger or smaller than that occupied by the swatch **1226**. The conventional electrode **150** may be positioned such that its hydrogel layer covers the release layer's opening **2122**. Those skilled in the art will also understand that either of the voided or conventional

electrodes **1200**, **150** may be mounted upon the side of the release liner **2100** upon which the swatch **2126** resides.

[208] FIG. **22B** is a cross sectional view of the voided electrode **2100** to release liner **2100** to conventional electrode **150** assembly **2202**, and FIG. **22C** is an equivalent circuit **2290** corresponding to or modeling the assembly **2202** of FIG. **22A**. In the equivalent circuit **2290**, a first circuit branch **2292** may correspond to a displacement current path outside a boundary defined by the release liner's swatch **2126** where it covers, fills, and/or blocks opening **2122**, in a manner analogous to that described above. Similarly, a second circuit branch **2294** may correspond to a displacement current path through an area or region in which the swatch **2126** covers, fills, and/or blocks the opening **2122**, in a manner analogous to that described above.

[209] The first circuit branch **2292** may include a resistance **R1a**, a capacitance **C1**, and a resistance **R1b**, and may be characterized by an impedance **Z1**. Resistance **R1a** may correspond to an effective resistance of the voided electrode's conductive foil areas and hydrogel layers **1220**, **1210** exclusive of areas in which the swatch **2126** covers, fills, and/or blocks the opening **2122**. Resistance **R1b** may correspond to an effective resistance of the conventional electrode's conductive foil and hydrogel layers exclusive of areas in which the swatch **2126** covers the opening **2122**. Capacitance **C1** may correspond to an effective capacitance of the release layer **2110** in areas excluding those in which the swatch **2126** covers the opening **2122**, and may be accounted for as a reactance **X1**. Impedance **Z1** may be decomposed or represented as $R1a + X1 + R1b$, in a manner analogous to that described above.

[210] The second circuit branch **2294** may include a resistance **R2a**, a capacitance **C2**, and a resistance **R2b**, and may be characterized by an impedance **Z2**. Resistance **R2a** may correspond to an effective resistance of the voided electrode's hydrogel layer **1210** in areas associated with the release liner's swatch **2126** where it covers, fills, and/or blocks the opening **2122** (i.e., an effective resistance of the voided electrode's hydrogel layer **1210** in an area in which the void **1222**, the hydrogel layer **1210**, the swatch **2126**, and the opening **2122** may be

coincident). Resistance R2b may correspond to an effective resistance of the conventional electrode's conductive foil and hydrogel layers in areas in which swatch **2126** covers the opening **2122**. Capacitance C2 may correspond to an effective capacitance of the swatch **2126** in an area or region in which the swatch **2126** covers, fills, overlaps, and/or blocks the opening **2122**, and may be accounted for as a reactance X2. Impedance Z2 may be decomposed or represented as $R2a + X2 + R2b$, in a manner analogous to that described above.

[211] In a manner analogous to that describe above, an effective impedance Z_{eff} may be defined as $((1/Z1) + (1/Z2))^{-1}$. Capacitance C2 may be significantly larger than capacitance C1 (i.e., $C2 \gg C1$); hence, reactance X2 is correspondingly much smaller than reactance X1. As a result, the second circuit branch **2294** provides a dominant current path relative to the first circuit branch **2292**. Furthermore, reactance X2 may be sufficiently small that it does not overwhelm or dominate the term $1/(R2a + X2 + R2b)$. Neither X1 nor X2 generally experience significant changes over time.

[212] R2a may correspond to a lateral or transverse current path through the voided electrode's hydrogel layer **1210**. As a result, R2a may be significantly larger than R2b. Moreover, R2a may exhibit a magnitude that is approximately equal to or in the same range as that of X2. As a result, changes in R2a over time, which may correspond to changes in the condition of the voided electrode's hydrogel layer **1210** over time, may significantly impact the effective impedance of the voided electrode **1200** to release layer **2100** to conventional electrode **150** assembly **2202**. Via measuring complex impedance measurement results over time, a medical device may determine an extent to which a voided electrode **1200** and/or a conventional electrode **150** mounted upon the release liner **2100** of FIG. 21A are optimal and/or fit for use. The medical device may provide an indication of electrode condition in manners described in detail below.

[213] FIG. 23A is a perspective view of a pair of voided electrodes **1200** of FIG. 12A mounted upon the release liner **2100** of FIG. 21A. Relative to FIGS. 12A and 21A, like reference numbers indicate like elements. The voided electrodes **1200** may be mounted upon each side of the release layer **2110**, thereby forming a voided

electrode **1200** to release liner **2100** to voided electrode **1200** assembly **2302**. One voided electrode **1200** may be mounted or positioned such that its void **1222** surrounds or encompasses the release liner's swatch **2126** in an area or region in which the swatch **2126** covers or fills the release layer's opening **2122**. Another voided electrode **1200** may be positioned on another side of the release layer **2110**, such that its void **1222** surrounds the release layer's opening **2122**.

[214] FIG. 23B is a cross sectional view of the voided electrode **1200** to release liner **2100** to voided electrode **1200** assembly **2302** of FIG. 23A, and FIG. 23C is an equivalent circuit **2390** corresponding to or modeling the assembly **2302** of FIG. 23A. In the equivalent circuit **2390**, a first circuit branch **2392** may correspond to a displacement current path outside a boundary defined by the release liner's swatch **2126** where it covers, fills, and/or blocks opening **2122**, in a manner analogous to that described above. Similarly, a second circuit branch **2394** may correspond to a displacement current path through an area or region in which the swatch **2126** covers, fills, and/or blocks the opening **2122**, in a manner analogous to that described above.

[215] The first circuit branch **2392** may include a resistance **R1a**, a capacitance **C1**, and a resistance **R1b**, and may be characterized by an impedance **Z1**. Resistances **R1a** and **R1b** may correspond to an effective resistance of a given voided electrode's conductive foil and hydrogel layers **1220**, **1210** exclusive of areas in which the swatch **2126** covers, fills, and/or blocks the opening **2122**. Capacitance **C1** may correspond to an effective capacitance of the release layer **2110** in areas excluding those in which the swatch **2126** covers the opening **2122**, and may be accounted for as a reactance **X1**. Impedance **Z1** may be decomposed or represented as $R1a + X1 + R1b$, in a manner analogous to that described above.

[216] The second circuit branch **2394** may include a resistance **R2a**, a capacitance **C2**, and a resistance **R2b**, and may be characterized by an impedance **Z2**. Resistances **R2a** and **R2b** may correspond to an effective resistance of a given voided electrode's hydrogel layer **1210** in areas associated with the release liner's swatch **2126** where it covers, fills, and/or blocks the opening **2122**, in a manner analogous to that previously described. Capacitance **C2** may correspond to an

effective capacitance of the swatch **2126** in an area or region in which it covers, fills, overlaps, and/or blocks the opening **2122**, and may be accounted for as a reactance X_2 . Impedance Z_2 may be decomposed or represented as $R_{2a} + X_2 + R_{2b}$, in a manner analogous to that described above.

- 5 **[217]** In a manner analogous to that describe above, an effective impedance Z_{eff} may be defined as $((1/Z_1) + (1/Z_2))^{-1}$, and an effective current I_{eff} may thus vary in accordance with $((1/Z_1) + (1/Z_2))$, or $(1/(R_{1a} + X_1 + R_{1b}) + 1/(R_{2a} + X_2 + R_{2b}))$. Capacitance C_2 may be significantly larger than capacitance C_1 , and hence reactance X_2 is correspondingly smaller than reactance X_1 . Additionally, reactance
- 10 X_2 may be sufficiently small that it does not overwhelm or dominate the term $1/(R_{2a} + X_2 + R_{2b})$. Neither X_1 nor X_2 generally experience significant changes over time.

- [218]** In the assembly **2302** of **FIGS. 23A** and **23B**, resistances R_{2a} and R_{2b} may correspond to lateral current paths through a hydrogel layer **1210**. Moreover, R_{2a} and R_{2b} may each exhibit a magnitude that is approximately equal to or in the
- 15 same range as that of X_2 . As a result, changes in R_{2a} and R_{2b} over time, which may correspond to changes in the condition of the voided electrodes' hydrogel layers **1210** over time, may significantly impact the effective impedance of the voided electrode **1200** to release layer **2100** to voided electrode **1200** assembly **2302**. Via measuring and/or recording complex impedance over time, a medical or
- 20 measurement device may determine an extent to which a voided electrode **1200** and/or a conventional electrode **150** mounted upon the release liner **2100** of **FIG. 21A** are optimal and/or fit for use. The medical device may provide an indication of electrode condition in manners described in detail below.

- [219]** **FIG. 24A** is a layered plan view of a release liner **2400** according to
- 25 another embodiment of the invention. The release liner **2400** comprises a nonconductive, non-stick release layer **2410** and a conductive backing layer **2460**. The release layer **2410** includes a first opening **2422**, a second opening **2432**, and a nonconductive swatch **2426** that covers, fills, overlaps, and/or blocks one of the openings **2422**, **2432**. The release layer **2410** and/or the conductive backing
- 30 layer **2460** may be implemented using materials previously described. The first and second openings **2422**, **2432** may be cut, stamped, or punched out of the release

layer **2410** in a conventional manner. In an alternate embodiment, one or both of the first and second openings **2422**, **2432** may comprise sets of openings. Finally, the swatch **2426** may comprise a thin material characterized by a high or generally high dielectric constant, such as a polymeric and/or ceramic material described above.

5 **[220]** The conductive backing layer **2460** may be adhered, laminated, and/or otherwise attached to the release layer **2410**, thereby maintaining or holding the backing layer **2460** in a given position. Additionally or alternatively, the conductive backing layer **2460** may be held in position by adhesion between the conductive backing layer **2460** and electrodes' hydrogel layers in regions defined by the release layer's openings **2422**, **2432**.

10 **[221]** **FIG. 24B** is a plan view of a conventional electrode **150** and a voided electrode **1200** of **FIG. 12** mounted upon the release liner **2400** of **FIG. 24A**. Relative to **FIGS. 12** and **24A**, like reference numbers indicate like elements. The voided electrode **1200** may be mounted upon the release layer **2410** such that its void **1222** surrounds the release layer's first opening **2422**, thereby surrounding at least a portion of the swatch **2426**. The conventional electrode **150** may be mounted upon the release layer **2410** such that its hydrogel layer covers the second opening **2422**.

15 **[222]** A medical or measurement device to which the voided and conventional electrodes **1200**, **150** are coupled may perform a complex impedance measurement in a manner analogous to that describe above with respect to **FIGS. 22A** and **22B**. Based upon the result of the impedance measurement, the medical or measurement device may provide an indication of electrical path condition and/or electrode condition or fitness for use, in manners described in detail below.

20 **[223]** **FIG. 25A** is a plan view of a release liner **2500** according to another embodiment of the invention. The release liner **2500** comprises a foldable release layer **2510** and a conductive backing layer **2560**. The foldable release layer **2510** may comprise a nonconductive, non-stick material such as those previously described. The foldable release layer **2510** includes a first mounting portion **2520** having a first opening **2522**; a second mounting portion **2530** having a second opening **2532**; a nonconductive swatch **2526** that covers, fills, overlaps, and/or

blocks the first openings **2522**; and a fold or midline region **2540**. The first and second openings **2522**, **2532** may be cut, stamped, or punched out of the release layer **2510** in a conventional manner. In an alternate embodiment, one or both of the first and second openings **2522**, **2532** may comprise sets of openings. The

5 conductive backing layer **2560** may be implemented using conventional materials in a manner analogous to that described above. Finally, the swatch **2526** may comprise a thin material characterized by a high or generally high dielectric constant, such as a polymeric and/or ceramic material described above.

[224] The foldable release layer **2510** may be folded, bent, or doubled in

10 either direction about its fold or midline region **2540** to surround or encase portions of the conductive backing layer **2560**. The backing layer **2560** may be adhered, laminated, and/or otherwise attached to the foldable release layer **2510**, thereby maintaining the conductive backing layer **2560** in a given position. Additionally or alternatively, in regions defined by the foldable release layer's openings **2522**, **2532**,

15 adhesion between the conductive backing layer **2560** and electrodes' hydrogel layers may hold the backing layer **2560** in position.

[225] FIG. **25B** is a perspective view of a pair of voided electrodes **1200** of FIG. **12A** mounted upon the release liner **2500** of FIG. **25A**. Relative to FIGS. **12A** and **25A**, like reference numbers indicate like elements. One voided electrode **1200**

20 may be mounted such that its void **1222** surrounds the first opening **2522** within the first mounting portion **2520**, thereby surrounding at least a portion of the swatch **2526**. Another voided electrode may be mounted such that its void **1222** surrounds the second opening **2532** within the second mounting portion **2530**. Voided electrodes **1200** mounted in the manner shown in FIG. **25B** reside upon an

25 identical side of the release layer **2510**, while the conductive backing layer **2560** may maintain contact with portions of another side of the release layer **2510**.

[226] A medical or measurement device coupled to voided electrodes **1200** mounted as shown in FIG. **25B** may perform a complex impedance measurement in a manner analogous to that describe above with respect to FIGS. **23A** and **23B**.

30 Based upon the result of the impedance measurement, the medical or measurement

device may provide an indication of electrical path condition and/or electrode condition or fitness for use, in manners described in detail below.

[227] FIG. 26 is a perspective view of a release liner **2600** according to another embodiment of the invention, and a pair of voided electrodes **1200** of FIG. 12A mounted thereupon. Relative to FIG. 12A, like reference numbers indicate like elements. In the embodiment shown, the release liner **2600** comprises a first release layer or sheet **2620**, a second release layer or sheet **2630**, and a conductive layer or medium **2660** disposed or residing therebetween. The first release layer **2610** includes a first opening **2622** and a swatch **2626** that covers, fills, overlaps, and/or blocks the first opening **2622**. The second release layer **2630** includes a second opening **2632** therein. The first and second release layers **2620** may comprise nonconductive, non-stick materials such as those previously described, and first and second openings **2622**, **2632** may be formed in conventional manners as previously described. The swatch **2626** may comprise a thin material characterized by a high dielectric constant, and may be formed or fabricated using polymeric and/or ceramic materials such as those described above.

[228] The conductive layer **2660** may comprise a sheet or layer of conductive material, such as an Aluminum or Tin foil layer, or a hydrogel layer. The conductive layer **2660** may be adhered, laminated, and/or otherwise attached one or both release layers **2620**, **2630**. Additionally or alternatively, the conductive layer **2660** may be held in position by hydrogel adhesion in regions in which the first and second release layers' openings **2622**, **2632** expose the conductive backing layer **2660** to the electrodes **1200**.

[229] One voided electrode **1200** may be mounted or positioned such that its void **1222** surrounds the first release layer's opening **2622**, thereby surrounding at least a portion of the swatch **2622**. Another voided electrode **1200** may be mounted such that its void **1222** surrounds the second release layer's opening **2632**. A medical device coupled to the voided electrodes **1200** mounted as shown in FIG. 26 may perform a complex impedance measurement in a manner analogous to that describe above with respect to FIGS. 23A and 23B. Based upon the result of the impedance measurement, the medical device may provide an indication of electrical

path condition and/or electrode condition or fitness for use, in manners described in detail below.

[230] In essentially any of the embodiments shown in **FIGS. 21A, 21B, 21C, 22A, 22B, 23A, 23B, 24A, 24B, 25A, 25B, and/or 26**, a swatch **2126, 2226, 2326, 2426, 2526, 2626** may be adhered, bonded, laminated, and/or otherwise attached to a release liner **2100, 2400, 2500, 2600**. Alternatively, direct attachment of a swatch **2126, 2226, 2326, 2426, 2526, 2626** to a release liner **2100, 2400, 2500, 2600** may be omitted. In such a situation, a swatch **2126, 2226, 2326, 2426, 2526, 2626** may be placed or positioned upon a release liner **2100, 2400, 2500, 2600** prior to placement or positioning of electrodes thereupon; or, a swatch **2126, 2226, 2326, 2426, 2526, 2626** may simply be appropriately positioned upon an electrode's hydrogel layer **1210** prior to placement or positioning of the electrode upon the release liner. Adhesion to an electrode's hydrogel layer **1210** may be sufficient to hold or maintain a swatch **2126, 2226, 2326, 2426, 2526, 2626** in a desired position. Upon removal from the release liner **2100, 2400, 2500, 2600**, the performance or behavior of the electrode **150, 1200** may be essentially unaffected provided that the swatch **2126, 2226, 2326, 2426, 2526, 2626** is sufficiently small.

[231] Variations upon the electrode/release liner embodiments above, such as those shown in **FIGS. 24B, 25B, and 26**, may exist. Such variations may involve other electrode embodiments, additional numbers of electrodes, and/or other release liner embodiments, in a manner consistent with the scope of the invention.

[232] As indicated above, a medical or measurement device coupled to electrodes mounted upon a release liner may test and/or characterize an electrical path associated with the mounted or packaged electrodes in a variety of manners. Furthermore, the medical or measurement device may provide various indications of electrode condition and/or fitness for use, as described in detail hereafter. In the context of the present invention, a medical device may comprise essentially any device capable of exchanging electrical signals and/or electrical energy with a patient's body via a set of electrodes, and may be, for example, an AED. Similarly, a measurement device may comprise essentially any type of device capable of

performing electrical measurements upon a set of electrodes mounted upon a release liner in accordance with the present invention.

[233] FIG. 27 is a block diagram of an AED 2700 coupled to electrodes 2794 mounted upon a release liner 2798 in accordance with an embodiment of the invention. The AED 2700 may comprise a power source or battery 2712; a power management unit 2714; an electrode signal management unit 2716; an electrode interface 2718; a first and a second gate array 2720, 2722; a memory 2730; a processing unit 2732; a communication interface or port 2734 that may be coupled to a data card 2736; an operator interface 2740 that includes a power or on/off switch 2742, a status indicator 2744, a display 2746, a contrast control 2748, a speaker 2750, a microphone 2752, a set of Light Emitting Diodes (LEDs) 2754, a shock button 2756, and an input interface 2758; a status measurement unit 2760; and a temperature sensor 2770.

[234] The electrode interface 2718 may be coupled via a connector 2710 to a plurality of electrodes 2794 mounted upon a release liner 2798. The release liner 2798 may be any type of structure that provides a non-stick surface upon which electrodes may be mounted, and which facilitates electrical characterization of electrical current path condition and/or electrode condition or fitness for use. The release liner 2798 may comprise any type of release liner embodiment described or disclosed herein. The electrodes 2794 may be of any type disclosed herein, and/or another type. Each electrode 2794 may include a corresponding lead wire 2796 that facilitates coupling to the connector 2710. The electrodes 2794 are operable to sense a patient's ECG (not shown) and deliver an electrical waveform, pulse, or shock when mounted upon a patient's body (not shown). The electrode signal management unit 2716 may manage signal and/or energy exchange between the electrodes 2794 and other AED elements via the electrode interface 2718. The electrode signal management unit 2716 may include impedance compensation circuitry, such as that referenced above.

[235] The status measurement unit 2760 may perform and/or direct periodic monitoring of various AED elements, systems, and/or subsystems, either automatically or in response to an AED operator's request. Operator requests may

be received via the input interface **2758**, which may include one or more buttons and/or a keypad. The status measurement unit **2760** may also direct the status indicator **2744** and/or the display **2746** to generate and/or present information or data to an AED operator corresponding to an operational condition of such AED elements, systems, and/or subsystems.

[236] The status measurement unit **2760** and/or the electrode signal management unit **2716** may include electrical measurement circuitry or elements that facilitate electrical path and/or electrode characterization in accordance with the present invention. The status measurement unit **2760**, possibly in conjunction with the memory **2730**, the data card **2736**, the processing unit **2732**, the first gate array **2720**, the second gate array **2722**, and/or the temperature sensor **2770** may periodically or continually initiate, manage, direct, and/or perform electrical path characterization operations to determine the status and/or operating condition of one or more portions of an electrical path defined by the connector **2710**, the lead wires **2796**, the electrodes **2794**, and the release liner **2798**. Based upon one or more temperature measurements received via the temperature sensor **2770**, the status measurement unit **2760** may adjust electrical measurement or test parameters to facilitate temperature compensated electrical characterization operations. The temperature sensor **2770** may comprise, for example, a thermocouple. One or more portions of the temperature sensor may be external to the AED **2700**.

[237] In one embodiment, one or more formulas or equations and/or data tables derived from and/or based upon empirical impedance versus temperature data may reside within the memory **2730**. Via insertion of a current or most-recent temperature measurement and a corresponding current or most-recent impedance measurement into an appropriate equation, the status measurement unit **2760** and/or the processing unit **2732** may determine an actual, corrected, or adjusted impedance value corresponding to mounted electrodes currently under consideration. An equation that provides corrected or adjusted impedance values in accordance with temperature and measured impedance values may be determined, for example, by standard curve-fitting techniques following empirical data acquisition. The status measurement unit **2760** and/or the processing unit **2732** may alternatively or

additionally rely upon one or more data tables to look up a corrected or adjusted impedance value corresponding to mounted electrodes currently under consideration. Those skilled in the art will recognize that a data table lookup procedure may return a closest or an interpolated value depending upon

5 implementation details.

[238] The status measurement unit **2760** may also periodically or continually initiate, perform, manage, and/or direct determination or calculation of one or more estimated or expected time intervals during which electrodes **2794** are likely to exhibit a given operating condition. Such determinations or calculations may be performed
10 in conjunction with the memory **2730**, the data card **2736**, the processing unit **2732** and/or one or both gate arrays **2720**, **2722**. The memory **2730** and/or the data card **2736** may store program instruction sequences for initiating, performing, and/or directing electrical path characterization operations. Finally, the status measurement unit **2760** may initiate or perform the aforementioned operations automatically or in
15 response to an AED operator's request.

[239] Electrical path characterization operations may include or involve temperature compensated impedance measurements such as those described herein, as well as generation, presentation, and/or provision of one or more indications of electrical path and/or electrode condition. Electrical path
20 characterization operations may involve stored data, such as electrical measurement results obtained or determined at one or more earlier times. Such stored data may be used, for example, to determine a present rate of change in electrode fitness, or an estimate thereof. Stored data may reside within the memory **2730**, and/or upon the data card **2736**.

[240] Based upon measurement results obtained and/or calculations or determinations made during the electrical path characterization operations, the status measurement unit **2760** may direct the status indicator **2744**, the display **2746**, the speaker **2750**, and/or the LEDs **2754** to generate and/or present status information and/or a set of messages to an AED operator. The status information and/or
30 messages may be in audible, textual, symbolic, and/or graphical formats.

[241] The status information and/or the messages may indicate that the electrical path is in adequate, acceptable, or good condition, or that one or more portions of the electrical path may be damaged or defective. Alternatively or additionally, the status information and/or the message may provide an indication of electrode condition or fitness for use. An AED operator may subsequently take appropriate action if required, such as replacement of packaged electrodes.

[242] In the event that an electrical path characterization operation and/or impedance measurement corresponds to a short or open circuit condition, a connector **2710**, a lead wire **2796**, an electrode **2794**, and/or one or more portions of the release liner **2798** may be damaged and/or defective. In such a case, the status measurement unit **2760** may direct the status indicator **2744**, the display **2746**, and/or the speaker **2750** to present a corresponding message or indication to an AED operator. Such a message may be, for example, "REPLACE ELECTRODES IMMEDIATELY."

[243] In the event that an electrical path characterization operation and/or impedance measurement results in a measured impedance value exceeding a given value or falling outside a given range, the status measurement unit **2760** may direct the status indicator **2744**, the display **2746**, and/or the speaker **2750** to generate and/or present a corresponding message, for example, "REPLACE ELECTRODES SOON." The status measurement unit **2760** or other element may additionally or alternatively generate a beep or other sound until electrode replacement has occurred.

[244] The status indicator **2744** may alternatively or additionally incorporate, generate, present and/or maintain one or more graphical or other type of visual metaphors that provide an indication of electrode condition and/or an expected amount of electrode lifetime remaining. Various types of indicators and/or interfaces for indicating electrode condition and/or an expected amount of electrode lifetime remaining are described in detail hereafter.

[245] FIG. 28A is an illustration of an electrode condition indicator **2800** in accordance with an embodiment of the invention. The electrode condition indicator **2800** may comprise a panel **2810** and an indicating element **2830**. The

panel **2810** may include a set of quality markings and/or regions **2812**, **2814**, **2816**, where each such region **2812**, **2814**, **2816** corresponds to an electrode operating condition or operating condition range. For example, the electrode condition indicator **2800** may include a first quality region **2812** corresponding to good or

optimal electrode condition; a second quality region **2814** corresponding to acceptable or fair electrode condition; and a third quality region **2816** corresponding to poor or unacceptable electrode condition. Other embodiments may incorporate additional or fewer quality regions. For example, in an alternate embodiment, an electrode condition indicator **2800** may include quality regions corresponding to an excellent quality or condition rating, a good quality or condition rating, an acceptable quality or condition rating, a poor quality or condition rating, and an unusable quality or condition rating. Any given quality region **2812**, **2814**, **2816** may include one or more color codings; and/or one or more quality regions **2812**, **2814**, **2816** may include text and/or symbols corresponding to an electrode operating condition.

The indicating element **2830** may comprise an arrow, needle, bar, or other type of element that may be positioned within any given quality region **2812**, **2814**, **2816**. Based upon electrical path characterization and/or impedance measurement results, the status measurement unit **2760** of FIG. 27 may issue signals to the electrode condition indicator **2800** to set or establish a given position for the indicating element **2830** relative to the quality regions **2812**, **2814**, **2816**. The indicating element's relative position may provide a fuel gauge metaphor for electrode condition and/or fitness for use. As electrode condition deteriorates over time, the indicating element **2830** may move into and/or through quality regions that correspond to poorer electrode fitness for use.

The indicating element **2830** may additionally or alternatively comprise or include a device or interface that changes color in response to changes in a surrounding environment, such as variations in relative humidity. The indicating element **2830** may incorporate one or more color references to convey a degree of reliability and/or an estimated usable electrode lifetime.

The electrode condition indicator **2800** may be implemented in a graphical manner upon an electrical interface such as a status indicator **2744** or

display **2746** of **FIG. 27**. Alternatively, the electrode condition indicator **2800** may be implemented as a physical interface that may comprise conventional electrical, mechanical, electro-mechanical, chemical, and/or electrochemical elements. Such a physical interface may form a portion, subsystem, or element of the status

indicator **2744**. For example, the panel **2810** may be implemented as a physical element within a corresponding housing (not shown), and the indicating element **2830** may be a piece of plastic and/or metal coupled to a shaft (not shown). The shaft may be coupled to a positioning device or actuator (not shown) that is responsive to signals received from the status measurement unit **2760** of **FIG. 27**.

[249] **FIG. 28B** is an illustration of an electrode condition indicator **2850** according to another embodiment of the invention. Relative to **FIG. 28A**, the electrode condition indicator **2850** of **FIG. 28B** may comprise corresponding, identical and/or essentially identical types of elements; hence, like reference numbers indicate like or corresponding elements. In the embodiment of **FIG. 28B**, the indicating element **2830** may comprise a bar that obscures, blocks, or covers one or more quality regions **2812**, **2814**, **2816** and/or portions thereof, successively exposing or blocking regions **2812**, **2814**, **2816** corresponding to poorer electrode condition or fitness for use over time in response to signals received via the status measurement unit **2760** of **FIG. 27**. The indicating element **2830** in such an embodiment may exhibit generally continuous or successive movement through one or more quality regions **2812**, **2814**, **2816** over time.

[250] **FIG. 29A** is an illustration of a remaining time indicator **2900** in accordance with an embodiment of the invention. The remaining time indicator **2900** may comprise a panel **2910** and an indicating element **2930**, in a manner analogous to that described above for the electrode condition indicator **2800** of **FIG. 28A**. The panel **2910** may include a set of regions and/or markings **2912**, **2914**, **2916**. Such markings may correspond to an estimated amount of time that an electrode may be likely to remain at a given performance or condition level, or an estimated amount of time remaining before electrode replacement is likely to be required.

[251] For example, a first marking **2912** may correspond to a duration of twelve months, while a second and a third marking **2914**, **2916** may correspond to a

duration of twenty four and thirty six months, respectively. Those skilled in the art will recognize that the first, second, and/or third markings **2912**, **2914**, **2916** may correspond to time periods other than those recited herein. Each region or marking **2912**, **2914**, **2916** may include associated text that indicates a time interval and/or a condition to which the region or marking **2912**, **2914**, **2916** corresponds. Each region or marking may also be color coded, in a manner analogous to that described above with reference to **FIG. 28A**.

[252] The indicating element **2930** may comprise an arrow, needle, bar, or other type of element that may be positioned upon, within, or between any given region or marking **2912**, **2914**, **2916**. Based upon 1) current and/or most-recent electrical path characterization and/or impedance measurement results; 2) prior electrical path characterization and/or impedance measurement results; and/or 3) empirical data characterizing hydrogel moisture loss, impedance measurement rates of change, and/or other factors that may affect electrode condition over time, the status measurement unit **2760** may issue signals to the remaining time indicator **2900** to set or establish a given position for the indicating element **2930** relative to the regions or markings **2912**, **2914**, **2916**.

[253] The position of the indicating element **2930** relative to the markings **2912**, **2914**, **2916** may convey, for example, that the electrodes have approximately X months left in an optimal performance zone, or Y months remaining until replacement is recommended or required, where determination of X and/or Y may be based upon a rate of change in current, prior, and/or empirical electrical properties. Electrical path property, characterization, and/or impedance measurement results, as well as the aforementioned empirical properties or data, may be stored within the memory of the AED **2700** of **FIG. 27**. The memory may include various types of nonvolatile and/or Read Only Memory (ROM) to facilitate efficient storage of such information.

[254] In a manner analogous to that for the electrode condition indicator of **FIG. 28A**, the position of the indicating element **2930** within the remaining time indicator **2900** relative to the regions or markings **2912**, **2914**, **2916** may provide a fuel gauge metaphor for an expected remaining electrode lifetime. As electrode

condition deteriorates over time, the indicating element **2930** may move through or past regions and/or markings **2912**, **2914**, **2916** that correspond to shorter or decreased expected electrode lifetime.

[255] The remaining time indicator **2900** may be implemented in a graphical manner upon an electrical interface such as a status indicator **2744** or display **2746** of **FIG. 27**. Alternatively, the remaining time indicator **2900** may be implemented as a physical interface that may comprise conventional electrical, mechanical, and/or electro-mechanical elements. Such a physical interface may form a portion, subsystem, or element of the status indicator **2744**. For example, the panel **2910** may be implemented as a physical element within a corresponding housing (not shown), and the indicating element **2930** may be a piece of plastic and/or metal coupled to a shaft (not shown). The shaft may be coupled to a positioning device or actuator (not shown) that is responsive to signals received from the status measurement unit **2760** of **FIG. 27**.

[256] **FIG. 29B** is an illustration of a remaining time indicator **2950** in accordance with another embodiment of the invention. Relative to **FIG. 29A**, the remaining time indicator **2950** of **FIG. 29B** may comprise corresponding, identical and/or essentially identical types of elements; hence, like reference numbers indicate like elements. In the embodiment of **FIG. 29B**, the indicating element **2930** may comprise a bar that obscures, blocks, or covers one or more regions or markings **2912**, **2914**, **2916** and/or portions thereof, successively exposing or blocking such markings **2912**, **2914**, **2916** to indicate diminishing expected electrode lifetime in response to signals received over time via the status measurement unit **2760** of **FIG. 27**.

[257] Any given electrode condition indicator **2800**, **2850** and/or remaining time indicator **2900**, **2950** may additionally or alternatively be incorporated into a packaged electrode structure. **FIG. 30** is a perspective view of a package **3000** in which an indicator **3080** and electrodes **3094** mounted upon a release liner **3098** reside. The electrodes **3094** and/or the release liner **3098** may be of a variety of types, including those described herein. Relative to **FIGS. 28A** and **29A**, like reference indicate like elements.

[258] The package **3000** may comprise a housing **3050** having a removable lid **3052** and an electrical interface **3060**, in a manner analogous to that described above in relation to **FIG. 4**. Electrodes **3094** mounted upon the release liner **3098** may be sealed within the package **3000**. The electrical interface **3060** may comprise a connector that facilitates electrical coupling of the electrodes **3094**, and possibly the indicator **3080**, to a medical device. The indicator **3080** may comprise an electrode condition indicator **2800**, **2850** and/or a time remaining indicator **2900**, **2950** such as those previously described. The indicator **3080** may reside within or upon the package **3000**.

[259] In one embodiment, the indicator **3080** may be coupled to a medical or measurement device, and thus the medical or measurement device may provide electrical power as well as measurement and/or computational capabilities required to indicate electrode fitness for use and/or an estimated duration associated with an electrode condition via the indicator **3080**. In an alternate embodiment, the indicator **3080** may comprise an electrode condition and/or time remaining indicator **2800**, **2850**, **2900**, **2950**, plus a control circuit **3082** and an independent power source **3084** such as a battery. The control circuit **3082** may include measurement, calculation, and/or processing elements necessary for determining an electrode condition and/or an estimated duration corresponding to electrode condition.

[260] A medical or measurement device may itself include an electrode condition and/or a time remaining indicator **3080** therein or thereupon. **FIG. 31** is a block diagram of an AED **3100** that includes an indicator **3080**. Relative to **FIGS. 27** and **30**, like reference numbers indicate like elements. The indicator **3080** may comprise an electrode condition and/or a time remaining indicator, which may be identical, essentially identical, and/or analogous to those described above with respect to **FIGS. 28A**, **28B**, **29A**, and/or **29B**.